

# Empirical Scatter Correction (ESC): A Universal CBCT Scatter Reduction Method without Prior Knowledge

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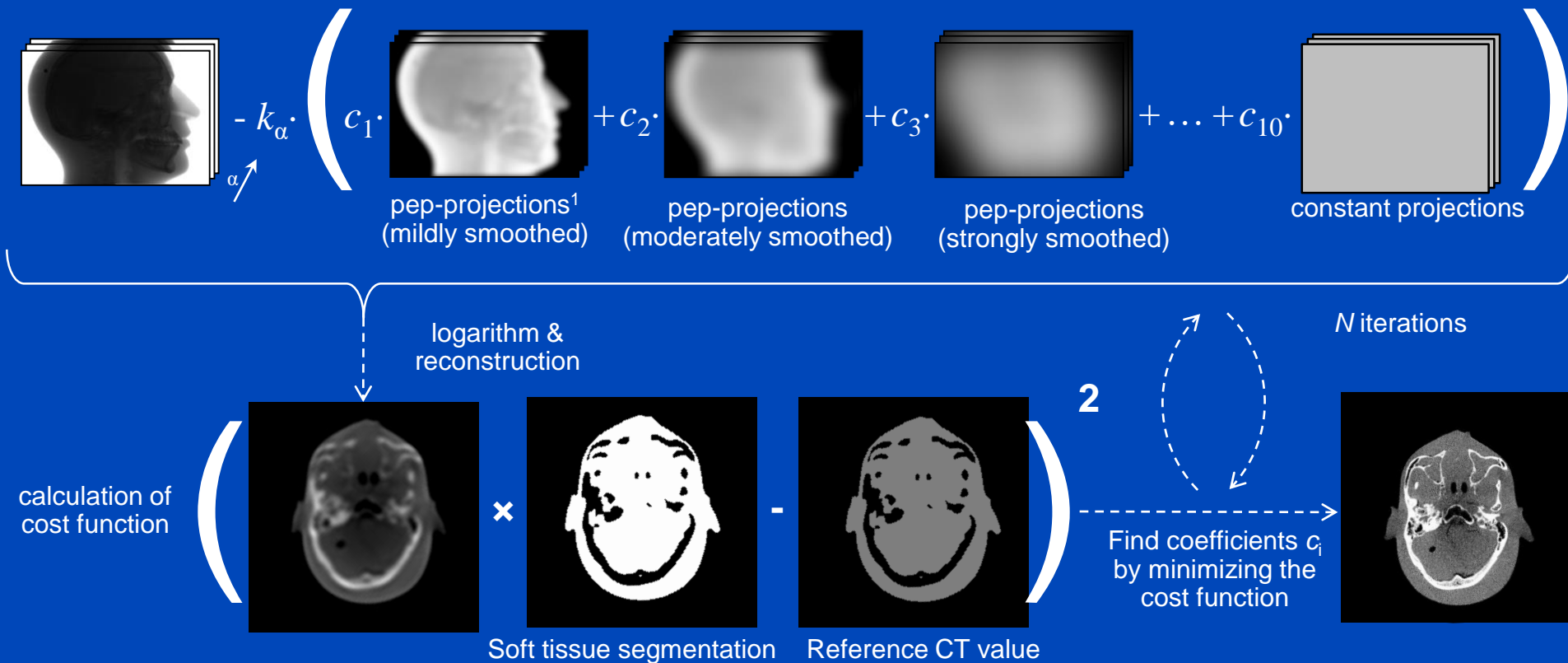
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**I do not have any conflict of interest to disclose.**

# Motivation & Aim

- Scatter is one of the most prominent sources of artifacts in cone-beam CT (CBCT).
- Software-based correction methods (kernel-based, Monte Carlo, Boltzmann, DSE, ...)\* rely on precise prior information about the object and the CT system.
- This prior knowledge may not always be available.
- **Aim:**  
**To provide a scatter correction algorithm that works without prior knowledge.**

# Method

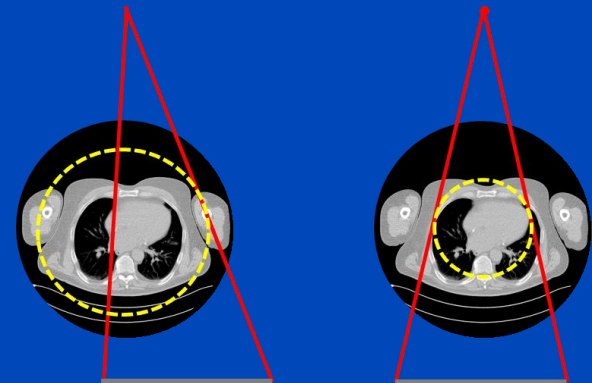


- **To reduce computation times: use subsampled projection data and reconstructions on a smaller voxel grid!**

$$k_\alpha = \begin{cases} \min \frac{I(u,v,\alpha)}{\sum_i c_i \cdot B_i(u,v,\alpha)} (1 - \delta) & \text{if } \min (I(u,v,\alpha) - \sum_i c_i \cdot B_i(u,v,\alpha)) < 0 \\ 1 & \text{else} \end{cases}$$

# Simulation Study

- Forward project diagnostic head, thorax, and abdomen CT scans into CBCT geometry.
- Add Monte Carlo-simulated scatter intensities.
- Simulate no ASG in order to obtain high SPRs.
- Geometries
  - Conventional cone-beam
  - Shifted-detector cone-beam
  - Truncated cone-beam (small detector)
- Compare with
  - MC-based scatter correction
  - Off-kV MC-based scatter correction (20 kV off)



# Results (Head)

scatter-free

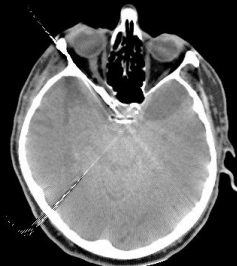
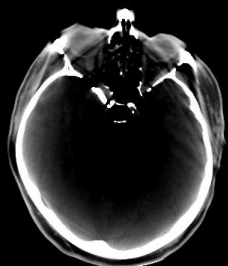
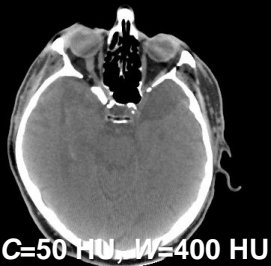
uncorrected

MC-corrected

off-kV MC-corrected

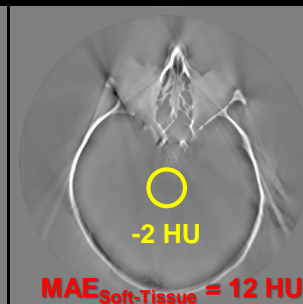
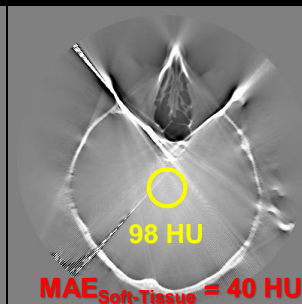
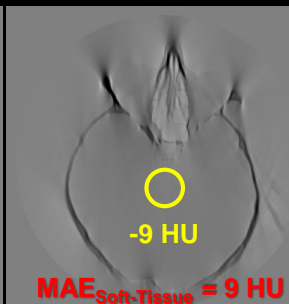
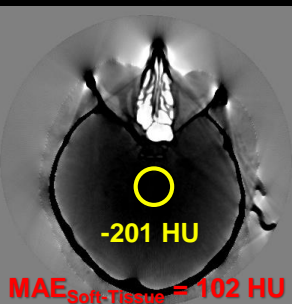
ESC-corrected

CT reconstruction

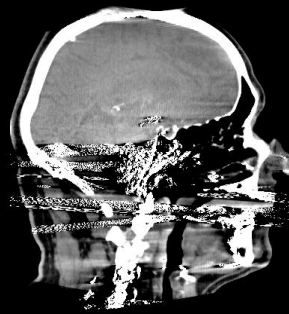
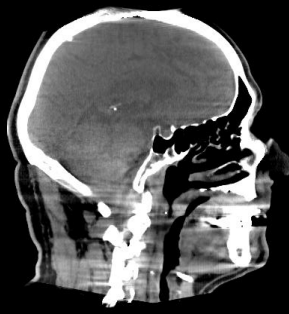


difference to scatter-free reconstruction

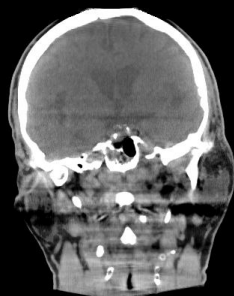
C=0 HU, W=400 HU



sagittal slice



coronal slice



# Results (Body)

shifted detector scans

truncated scans

scatter-free

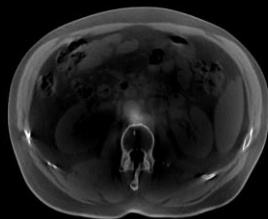
uncorrected

ESC-corrected

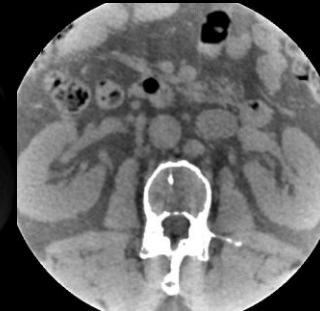
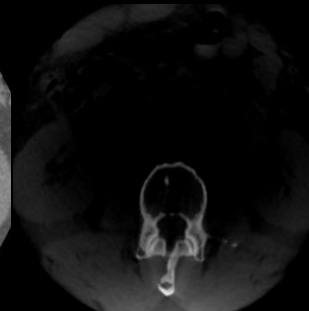
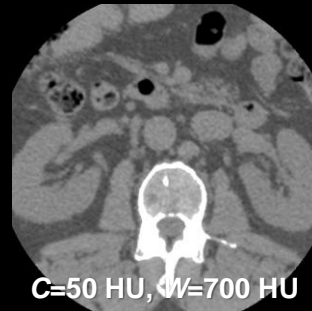
scatter-free

uncorrected

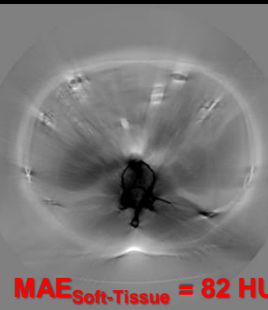
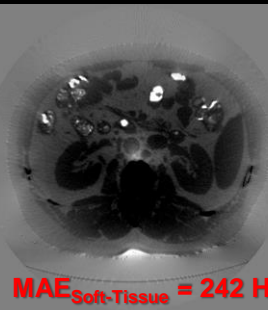
ESC-corrected



C=50 HU, W=700 HU



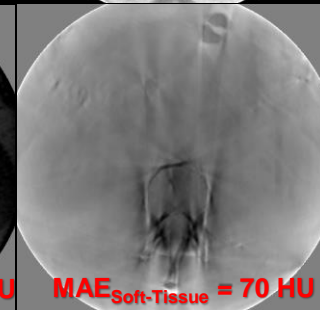
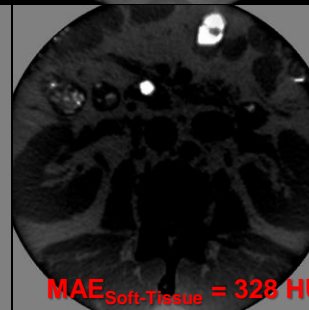
C=50 HU, W=700 HU



C=0 HU, W=700 HU

MAE<sub>Soft-Tissue</sub> = 242 HU

MAE<sub>Soft-Tissue</sub> = 82 HU



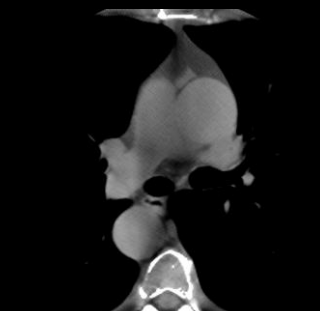
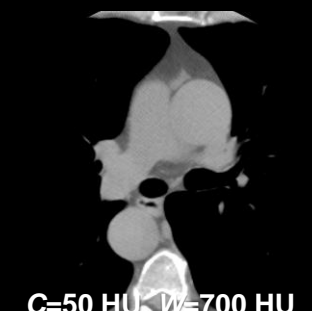
C=0 HU, W=700 HU

MAE<sub>Soft-Tissue</sub> = 328 HU

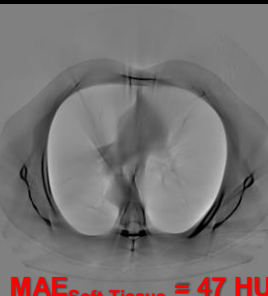
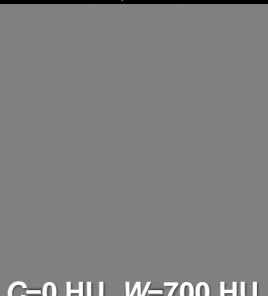
MAE<sub>Soft-Tissue</sub> = 70 HU



C=50 HU, W=700 HU



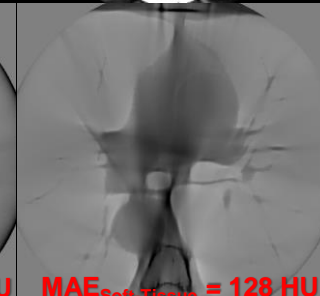
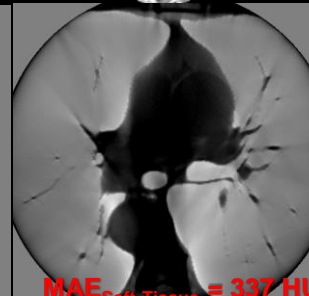
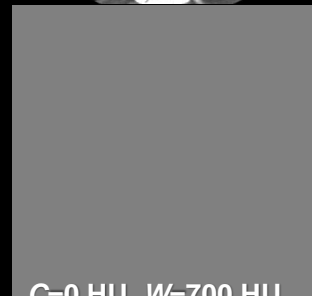
C=50 HU, W=700 HU



C=0 HU, W=700 HU

MAE<sub>Soft-Tissue</sub> = 205 HU

MAE<sub>Soft-Tissue</sub> = 47 HU



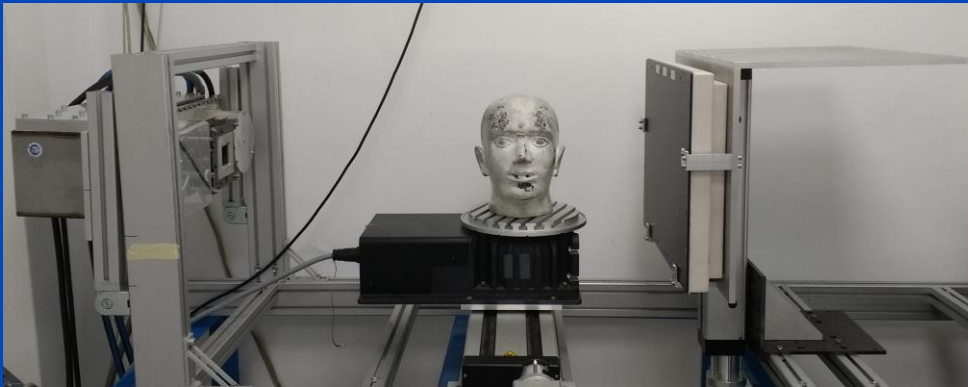
C=0 HU, W=700 HU

MAE<sub>Soft-Tissue</sub> = 337 HU

MAE<sub>Soft-Tissue</sub> = 128 HU

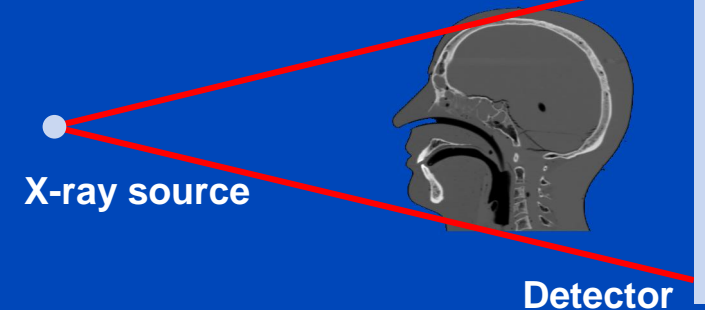
# Phantom Measurement

## DKFZ table-top CT

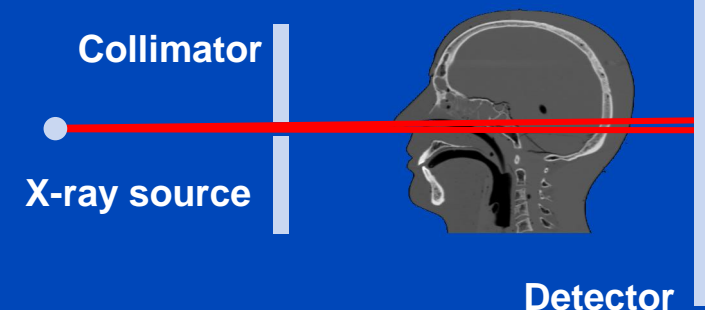


- Measurement of a head phantom at our in-house table-top CT.
- Slit scan measurement serves as ground truth.
- Scan parameters:
  - $U = 120 \text{ kV}$  (9 mm Al)
  - $P = 360 \text{ W}$

### Measurement to be corrected

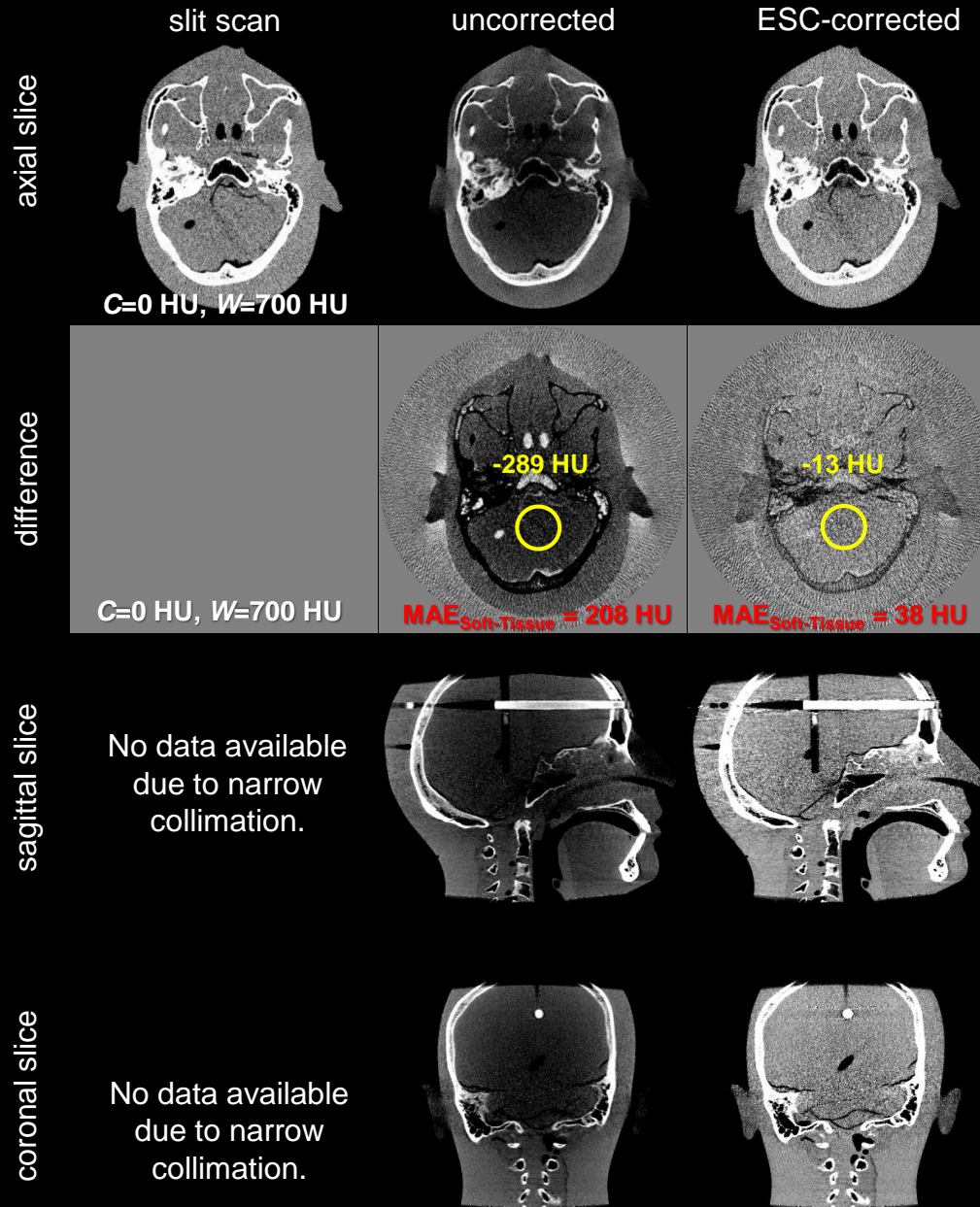


### Ground truth: slit scan





# Results (Measured Phantom)



# Conclusions

- ESC is able to improve image quality in CBCT simulations and measurements without specific prior knowledge.
- In some cases the remaining artifacts may be higher than with optimized solutions that use prior knowledge.
- The computation time of ESC is in the order of one to two minutes. Optimizations may include a Taylor expansion from intensity to log domain.

# Thank You!

This presentation is available at [www.dkfz.de/ct](http://www.dkfz.de/ct)

This work was supported in parts by the BMBF under grant number 13N14804.

Job opportunities through DKFZ's international PhD or Postdoctoral Fellowship programs ([www.dkfz.de](http://www.dkfz.de)), or directly through Prof. Dr. Marc Kachelrieß ([marc.kachelriess@dkfz.de](mailto:marc.kachelriess@dkfz.de)).

Parts of the reconstruction software were provided by RayConStruct® GmbH, Nürnberg, Germany.