

Five-Dimensional Respiratory and Cardiac Motion Compensation for Simultaneous PET/MR

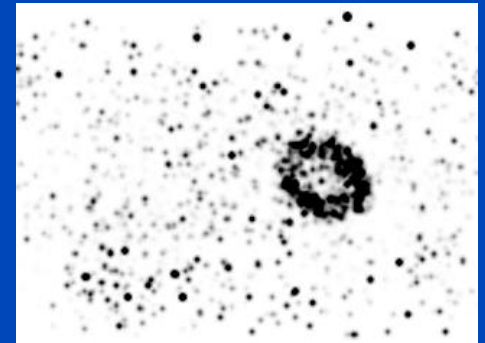
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Introduction

- One major challenge in PET image reconstruction is respiratory and cardiac patient motion
- Motion causes image blurring and an underestimation of the reconstructed activity
- Gating
 - sort data into respiratory and cardiac bins and reconstruct data from each bin separately
 - trade-off between temporal resolution and an appropriate SNR and CNR of the PET images
- **Recent approach: PET/MR motion compensation (MoCo)^{1,2,3}**
 - use MR information to estimate motion vector fields (MVF)
 - MoCo PET reconstruction from 100% of raw data

5D double-gated PET



[1] Petibon et al. Cardiac motion compensation and resolution modeling in simultaneous PET-MR: A cardiac lesion detection study. *Phys Med Biol* 2013.

[2] Huang et al. Accelerated acquisition of tagged MRI for cardiac motion correction in simultaneous PET-MR: phantom and patient studies. *Med Phys* 2015.

[3] Munoz et al. MR-based cardiac and respiratory motion-compensation techniques for PET-MR imaging. *PET Clin* 2016.

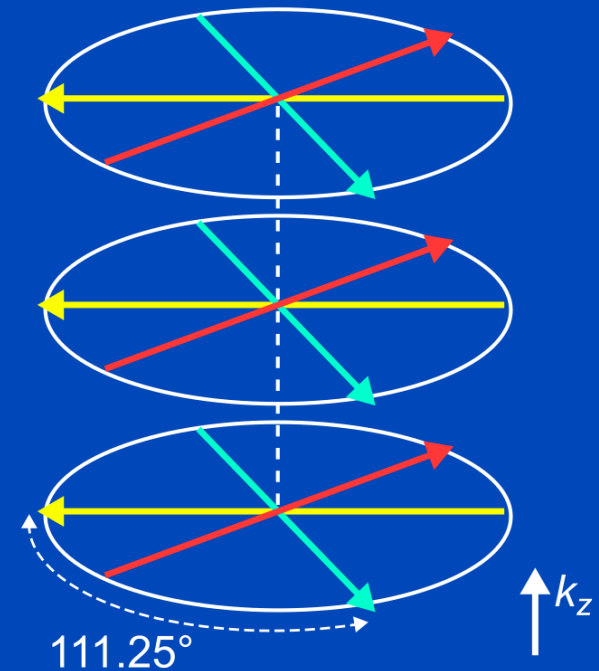
Aim of Work

- Develop a method for respiratory and cardiac motion compensation of PET images
- Use information from simultaneously acquired MR data for motion estimation
- Difficulty: efficient and robust estimation of both respiratory and cardiac MVFs



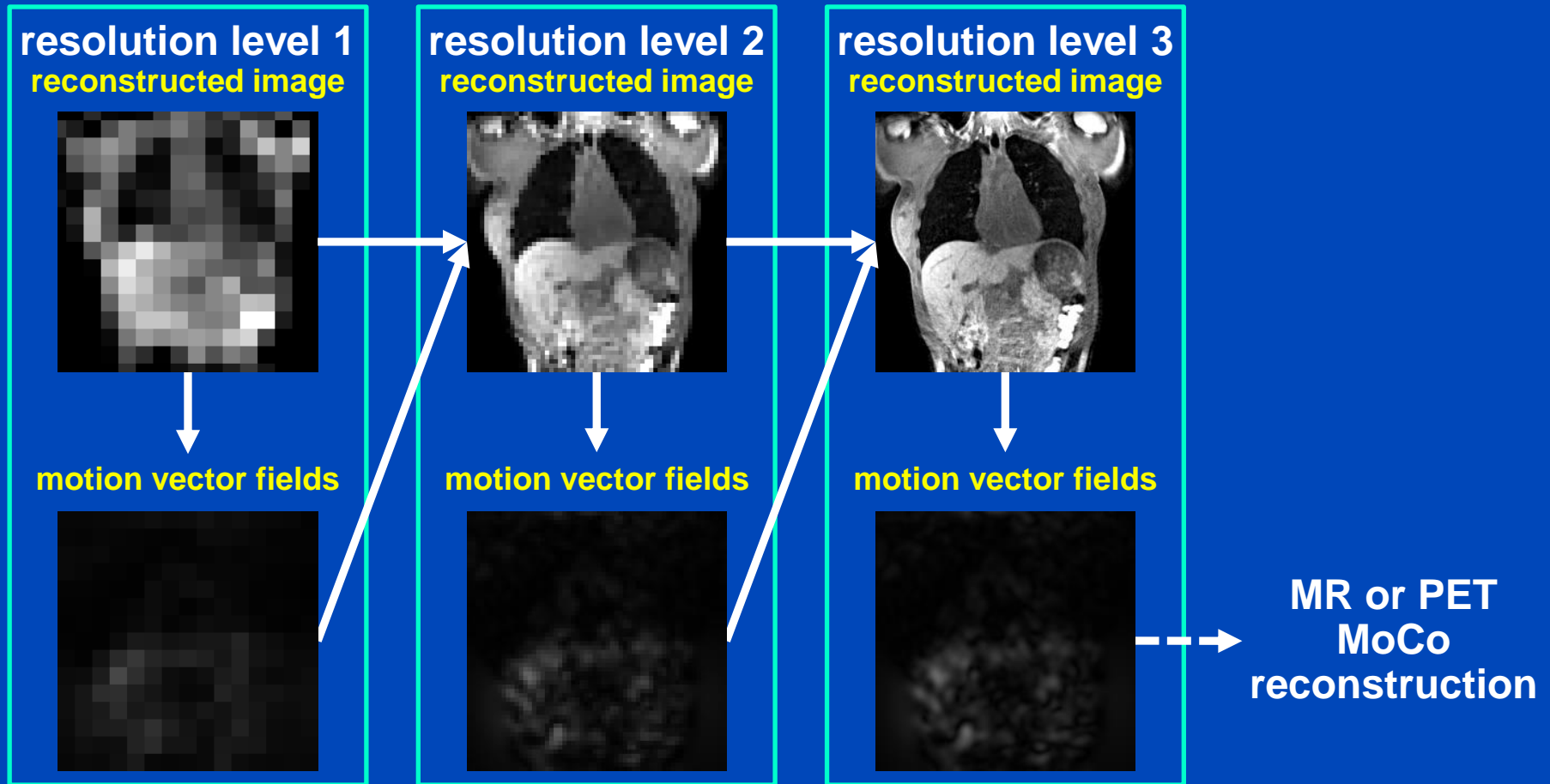
Data Acquisition and Processing

- Simultaneous PET/MR acquisition with 5 min per bed (Biograph mMR, Siemens Healthineers)
- Tracer: fluorodeoxyglucose (^{18}F -FDG)
- 3D-encoded gradient echo sequence with radial stack-of-stars sampling
- Golden angle ($\approx 111.25^\circ$) radial spacing
- Intrinsic estimation of motion signals
- MR and PET data were sorted into 20 overlapping respiratory motion phases (10% width) and 12 overlapping cardiac motion phases (17% width)



Algorithm for Motion Estimation

4D joint MoCo-HDTV¹



Algorithm for Motion Estimation

MR Image Reconstruction - Cost Function^{1,2}

- **Cost function:**

$$C = \underbrace{\|X_{pc} S f - p\|_2^2}_{\text{raw data fidelity}} + \underbrace{\mu \text{HDTV } f}_{\text{total variation}}$$

X_{pc} : motion phase-correlated forward transform
 S : coil sensitivity profiles
 f : 4D image volume
 p : measured raw data
 μ : weight
HDTV : spatial and temporal total variation

- The first term optimizes the raw data fidelity
- The second term improves the image sparsity by optimizing the spatial and temporal total variation
- Both terms are optimized in an alternating manner
- The cost function is optimized for the complete 4D volume including all motion phases

[1] Ritschl, Sawall, Knaup, Hess, Kachelrieß. Iterative 4D cardiac micro-CT image reconstruction using an adaptive spatio-temporal sparsity prior. *Phys. Med. Biol.* 2012.

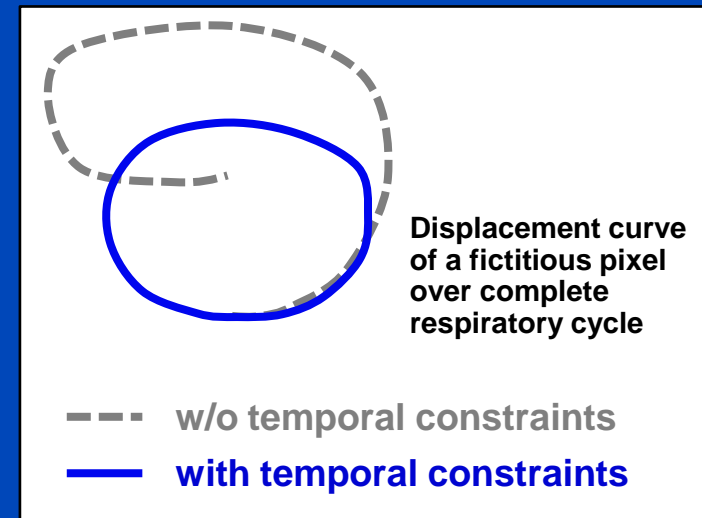
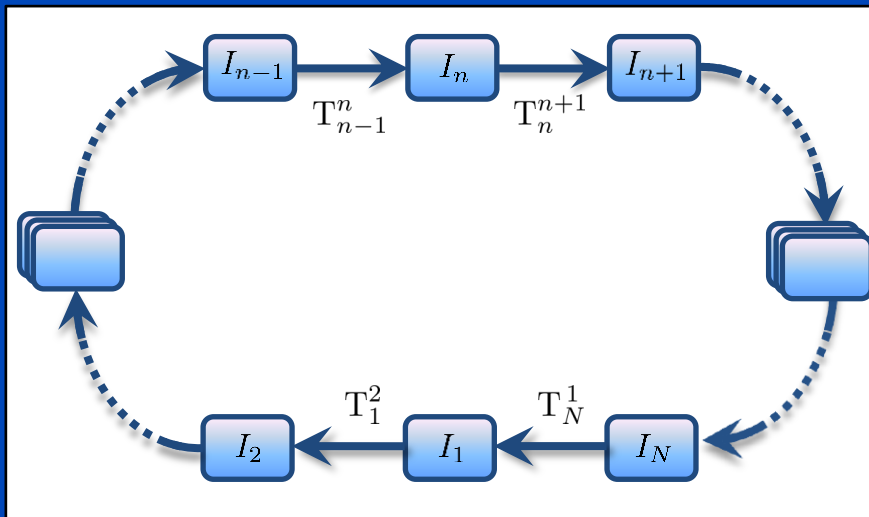
[2] Rank, Heußler, Buzan, Wetscherek, Freitag, Dinkel, Kachelrieß. 4D respiratory motion-compensated image reconstruction of free-breathing radial MR data with very high undersampling.

Magn Reson Med, early view online.

Algorithm for Motion Estimation

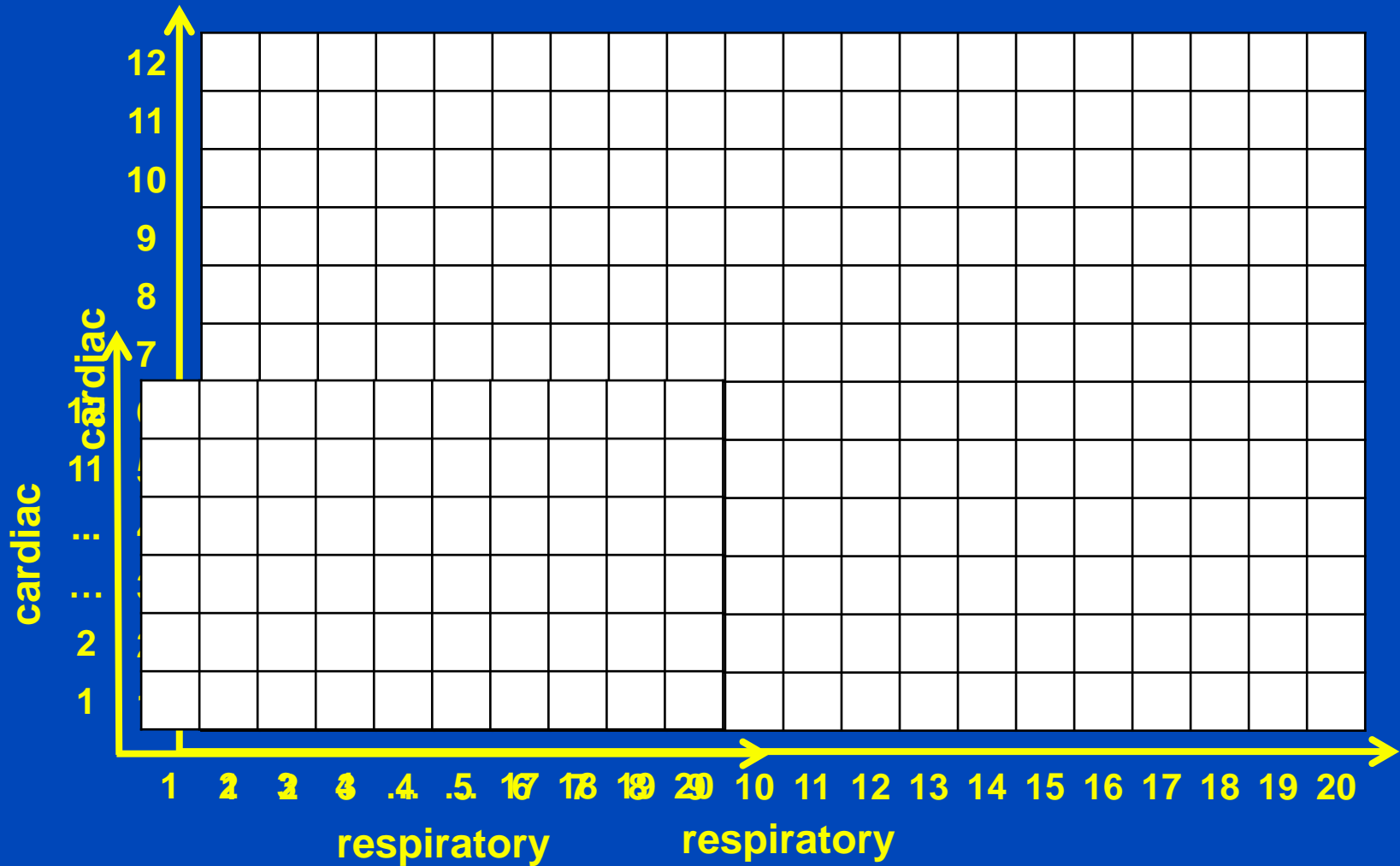
Cyclic Deformable Registration¹

- Motion estimation only between adjacent phases
 - all other motion vector fields given by concatenation



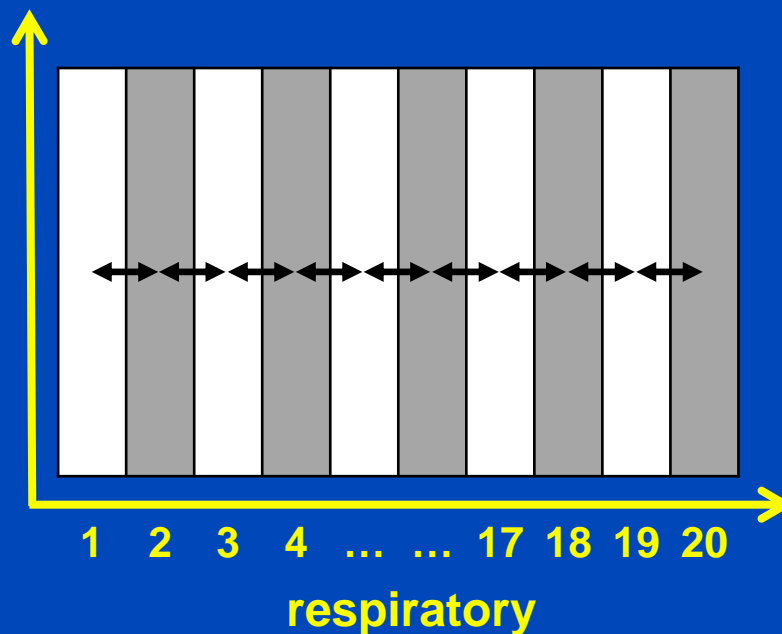
- Incorporate additional knowledge
 - a priori knowledge of quasi periodic breathing pattern
 - non-cyclic motion is penalized
 - error propagation due to concatenation is reduced

Double-Gated Raw Data Matrix



Respiratory Motion Estimation

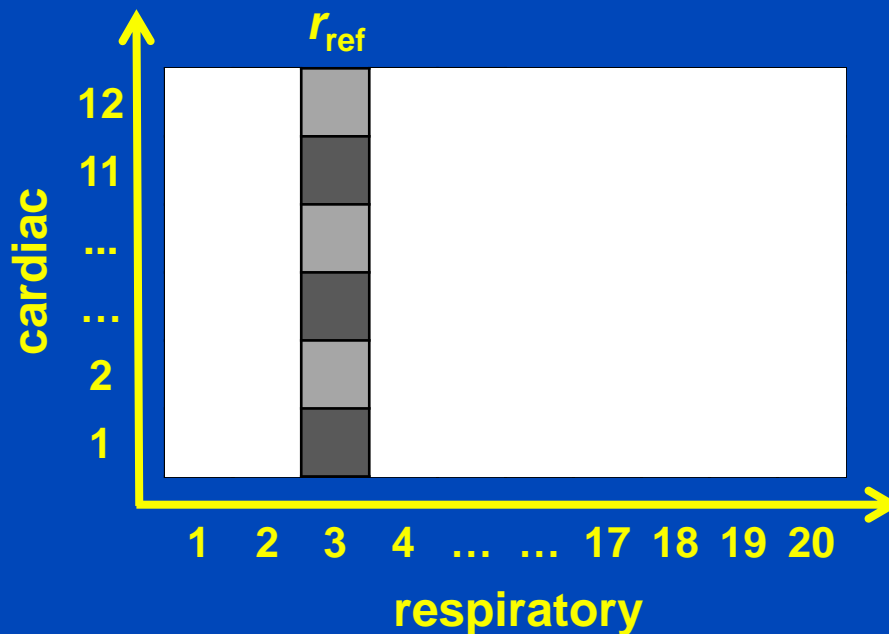
- Respiratory MVFs are estimated neglecting the effect of cardiac motion
- The 4D joint MoCo-HDTV¹ algorithm is employed for motion estimation in the respiratory dimension



Generation of Respiratory MoCo MR Raw Data

- Respiratory MoCo MR raw data for cardiac phase c at the respiratory reference phase:

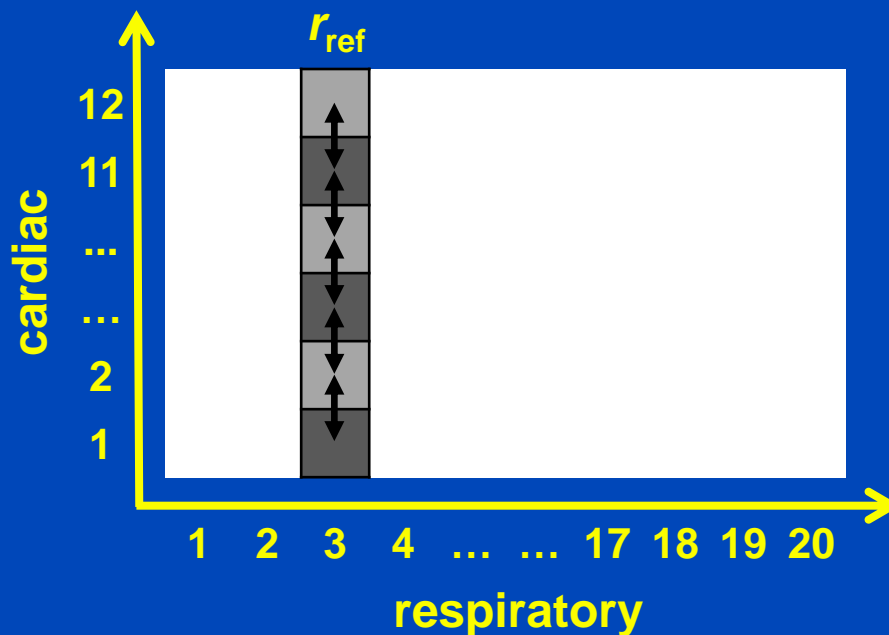
$$p_{r_{\text{ref}},c}^{\text{resp MoCo}} = X \sum_r D_r^{r_{\text{ref}}} X^\dagger G_r G_c p$$



- r, c : indices of respiratory and cardiac phases
- X, X^\dagger : forward and pseudo-inverse transform
- $D_r^{r'}$: warping operation mapping volume of phase r' to r
- G_r, G_c : gating operators
- p : measured raw data

Cardiac Motion Estimation

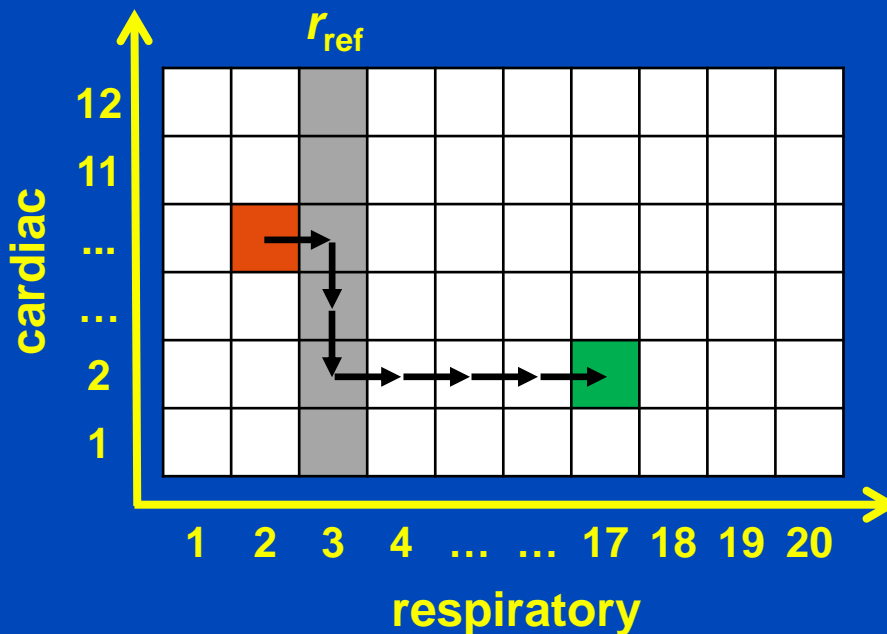
- Cardiac MVFs are estimated for the respiratory MoCo MR raw data at the respiratory reference phase
- The 4D joint MoCo-HDTV¹ algorithm is employed for motion estimation in the cardiac dimension



5D MoCo MR Reconstruction

- Employing 5D double-gated MR images, any arbitrary combination of respiratory and cardiac phase can be reconstructed:

$$f_{r,c} = \sum_{r',c'} D_{r',c'}^{r,c} S^\dagger X^\dagger G_{r'} G_{c'} p$$

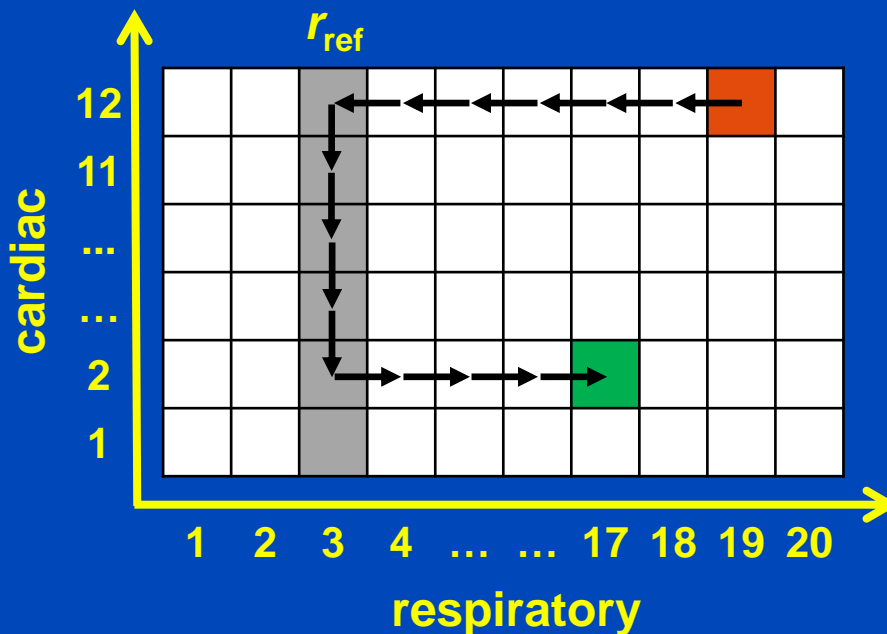


- r, c : indices of respiratory and cardiac phases
- $D_{r',c'}^{r,c}$: warping operation mapping volume of phase (r',c') to (r, c)
- S^\dagger : coil combination
- X^\dagger : pseudo-inverse transform
- G_r, G_c : gating operators
- p : measured raw data

5D MoCo MR Reconstruction

- Employing 5D double-gated MR images, any arbitrary combination of respiratory and cardiac phase can be reconstructed:

$$f_{r,c} = \sum_{r',c'} D_{r',c'}^{r,c} S^\dagger X^\dagger G_{r'} G_{c'} p$$



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- S^\dagger : coil combination
- X^\dagger : pseudo-inverse transform
- G_r, G_c : gating operators
- p : measured raw data

5D MoCo PET Reconstruction

- MoCo OSEM update equation of subiteration $i+1$ and motion phase (r, c) :

$$\lambda_{r,c,(i+1)} = \lambda_{r,c,(i)} \frac{1}{N_c \sum_{r',c'} D_{r',c'}^{r,c} M_k^T \left(\frac{1}{a_{r',c'}} \right)} \sum_{r',c'} D_{r',c'}^{r,c} M_k^T \frac{G_{r'} G_{c'} p}{(M_k D_{r',c'}^{r',c'} \lambda_{r',c',(i)} + a_{r'}(dn + s))}$$

- Parameters:**

- 3 iterations, 21 subsets
- Gaussian smoothing with FWHM = 3.2 mm after each iteration

i :	subiteration index
k :	subset index: $k = i \bmod K$
r, r' :	indices of respiratory motion phases
c, c' :	indices of cardiac motion phases
M_k, M_k^T :	system matrix including forward-/backprojection of subset k
p :	measured raw data
d :	estimated randoms
s :	estimated scatter
$\lambda_{(i)}$:	image estimate at subiteration i
$D_{r',c'}^{r,c}$:	warping operation mapping volume of phase (r',c') to (r, c)

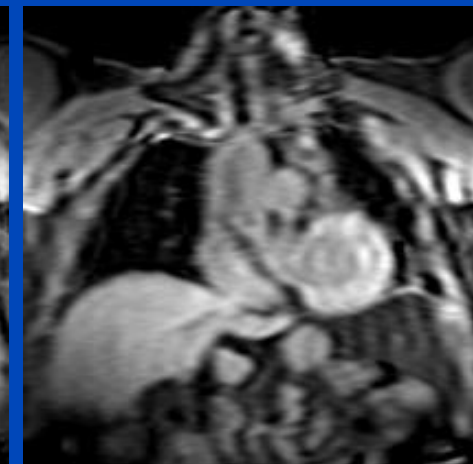
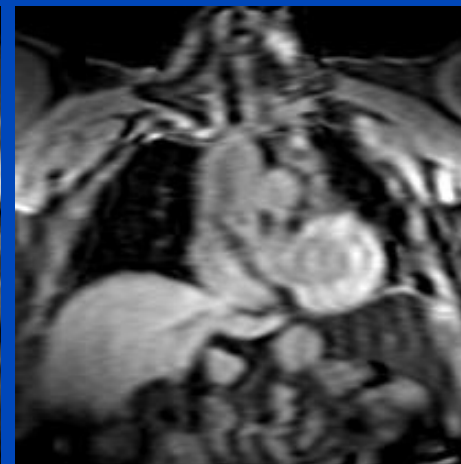
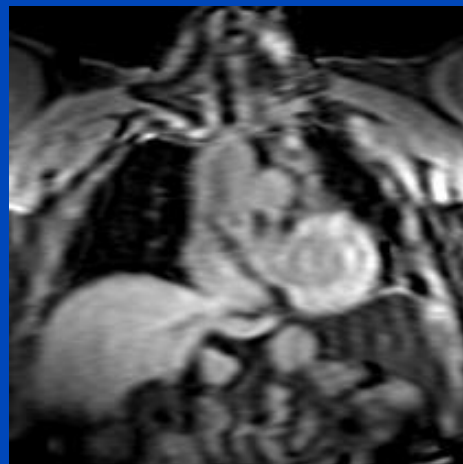
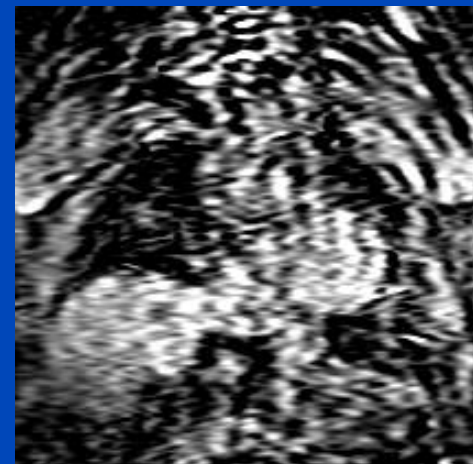
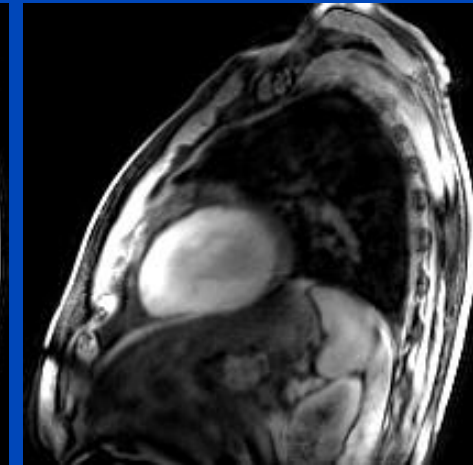
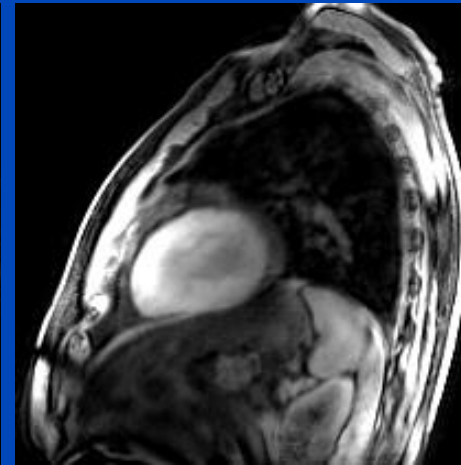
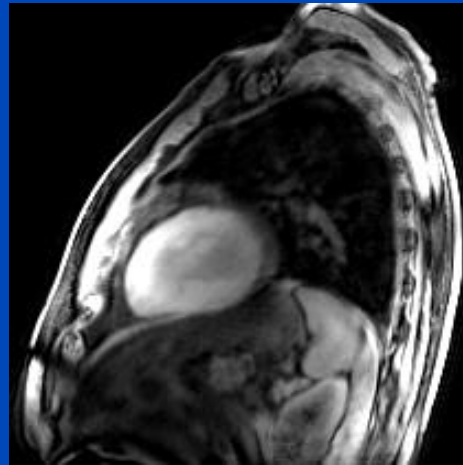
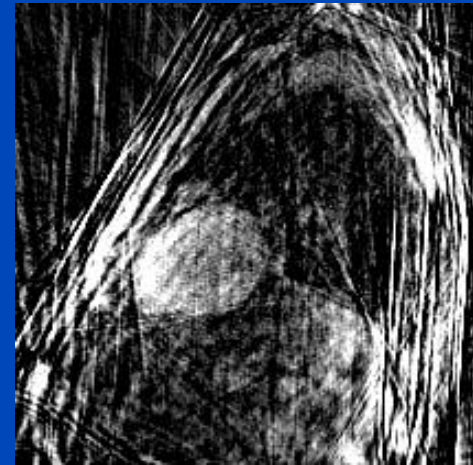
Results of 5D MR Reconstructions

5D double-gated MR
r = 1, *c*-loop

5D MoCo MR
r = 1, *c*-loop

5D MoCo MR
r-loop, *c* = 1

5D MoCo MR
r-loop, *c*-loop



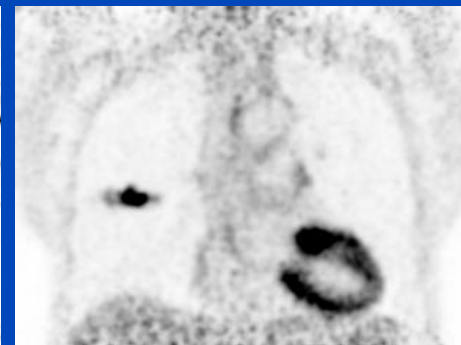
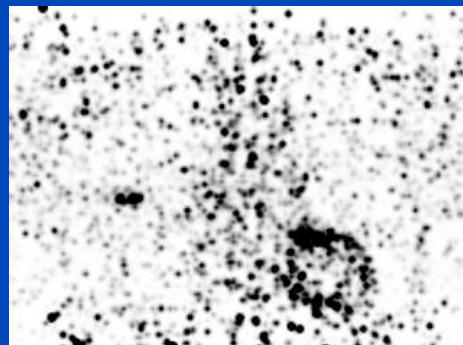
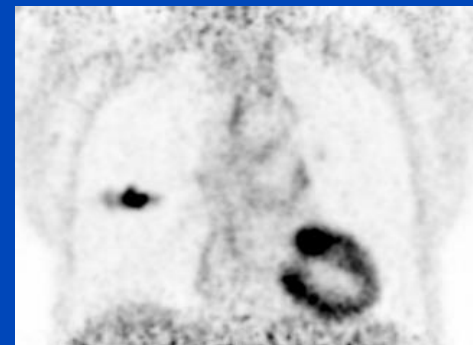
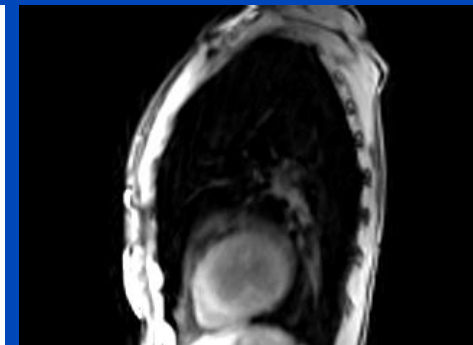
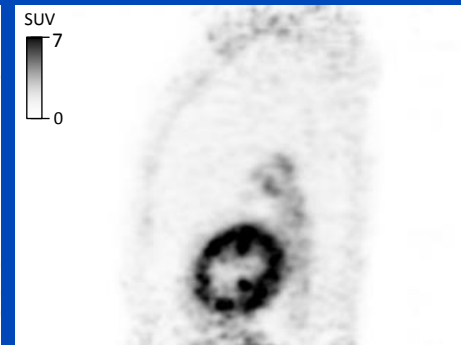
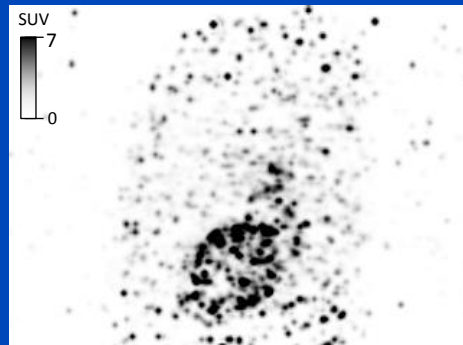
Results of 5D PET Reconstructions (I)

3D PET
motion average

5D double-gated PET
 $r = 1$, c-loop

5D MoCo PET
 $r = 1$, c-loop

5D MoCo MR
 $r = 1$, c-loop

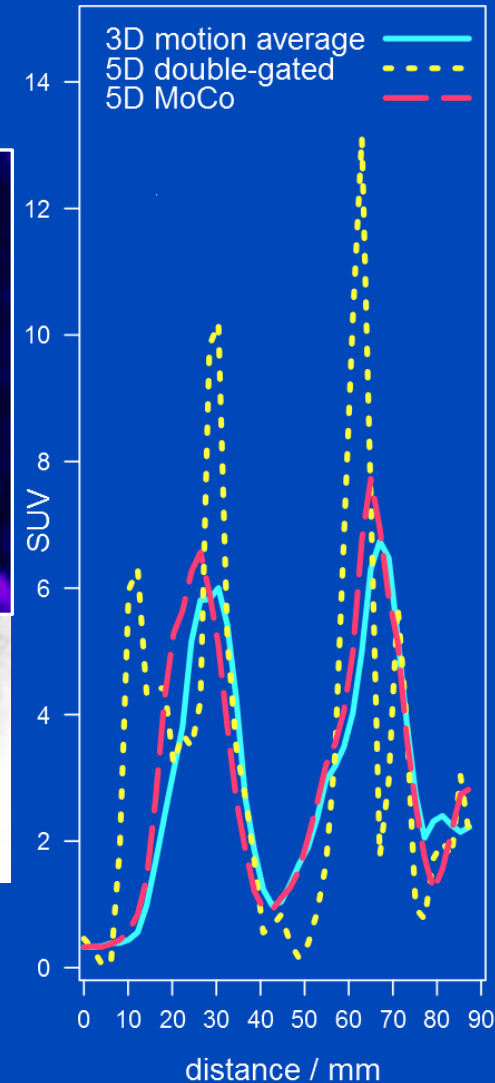
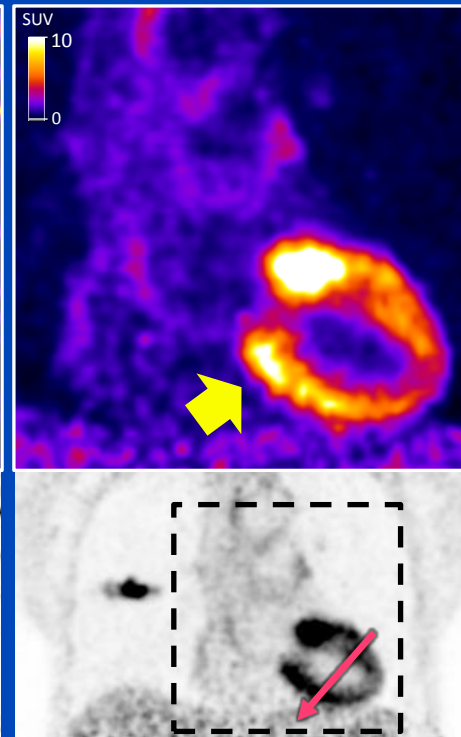
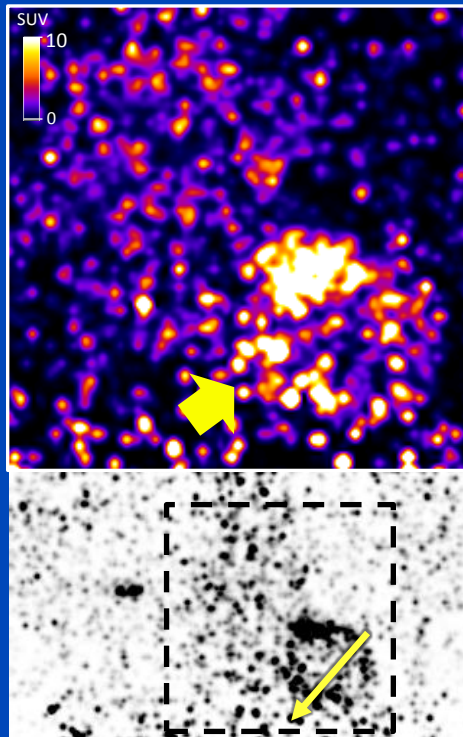
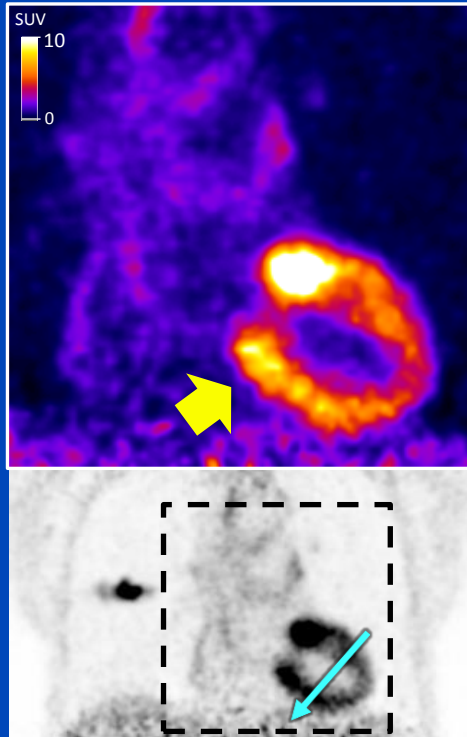


Results of 5D PET Reconstructions (II)

3D PET
motion average

5D double-gated PET
 $r = 1$, end-diastole

5D MoCo PET
 $r = 1$, end-diastole



Summary and Outlook

- Novel method which sequentially estimates respiratory and cardiac MVFs from MR data
- 5D MoCo allows for PET or MR reconstruction of any arbitrary combination of respiratory and cardiac phase
- MoCo for PET improves PET quantification, image sharpness and noise level
- **Next steps:**
 - Verification of results with patients having cardiac disease
 - Optimization of workflow and performance

Thank You!



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Conference Chair

Marc Kachelrieß, German Cancer Research Center (DKFZ), Heidelberg, Germany

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This presentation will soon be available at www.dkfz.de/ct.

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