

Reanimating Patients using Motion Transfer: A Cardiorespiratory Motion Ground Truth Based on Clinical CT Patient Data

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Introduction

- **Motion compensation (MoCo) is an important tool in medical imaging.**



3D CBCT

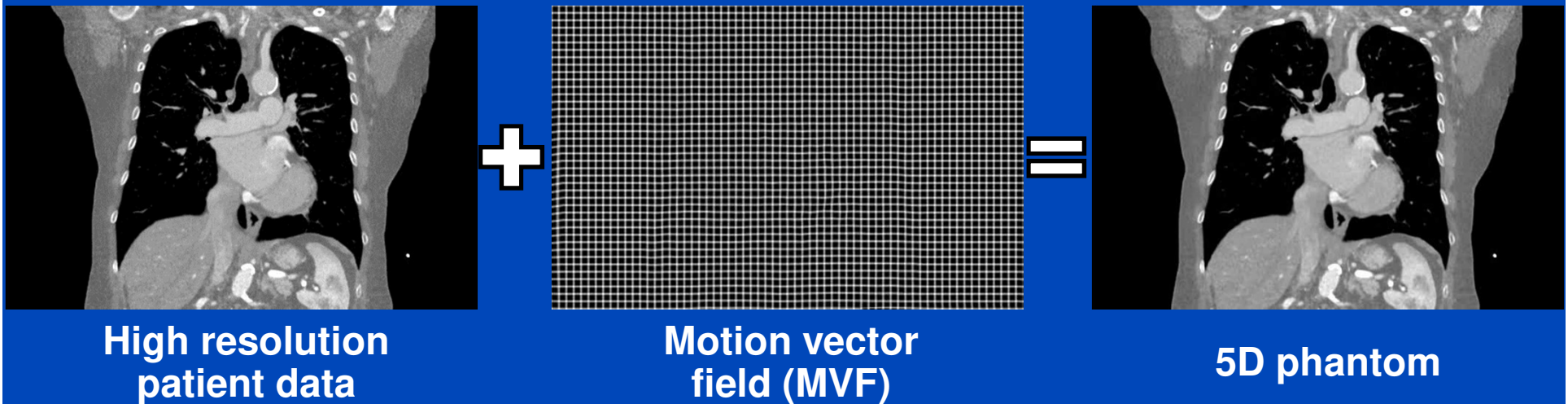


5D MoCo

- **Hard to assess algorithms quantitatively as there is no motion ground truth available.**

Aims

- Generate motion phantoms based on voxelized patient data.
- Provide 4D and 5D motion ground truth (GT) patient data including motion information.



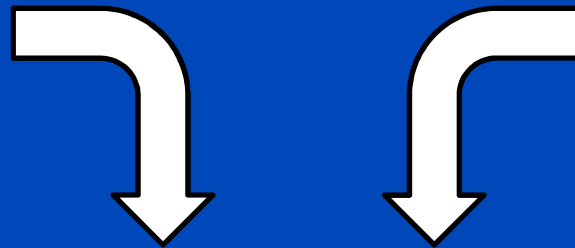
$C = 0 \text{ HU}, W = 1400 \text{ HU}$

Motion Transfer

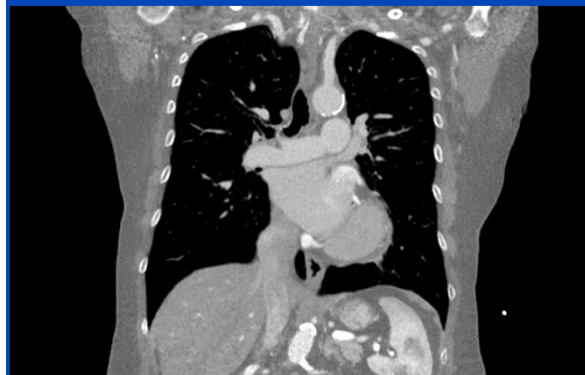


4D respiratory source

Transfer motion to static destination patient anatomy

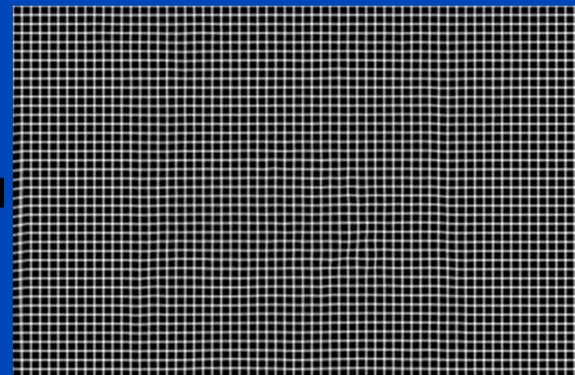


4D cardiac source



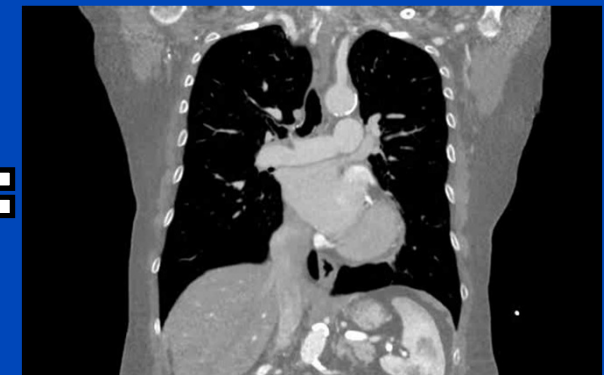
High resolution patient data

+



Motion vector field (MVF)

=



5D phantom

$C = 0 \text{ HU}, W = 1400 \text{ HU}$

Motion Transfer with Deformable Image Registration

1. Motion extraction

$f_t(\mathbf{r})$ Motion data (phase t)
in source anatomy

$\mathbf{m}_t(\mathbf{r})$ Motion vector fields
(MVF s)

$$f_t(\mathbf{r}) = f_0(\mathbf{m}_t(\mathbf{r}))$$

2. Anatomy matching

$g_0(\mathbf{r})$ Static patient data in
destination anatomy

$d(\mathbf{r})$ Anatomy map relating
both anatomies

$$g_0(\mathbf{r}) \doteq f_0(d(\mathbf{r}))$$

3. MVF transfer

$$\tilde{\mathbf{m}}_t(\mathbf{r}) = d^{-1}(\mathbf{m}_t(d(\mathbf{r})))$$

$$g_t(\mathbf{r}) = g_0(\tilde{\mathbf{m}}_t(\mathbf{r}))$$

Cardiac Reanimated Destination Patient

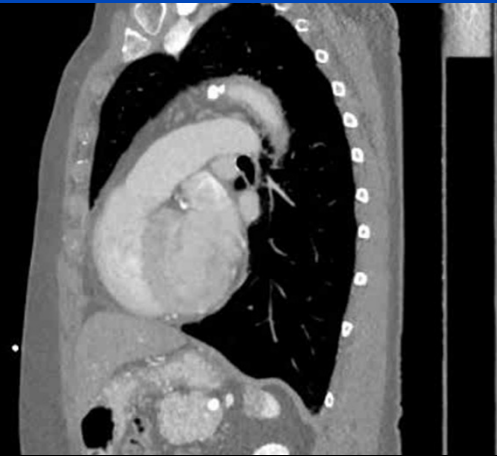
- We successfully applied the approach to cardiac motion.
- A well-regularized anatomy map leads to realistic cardiac motion transfer.



axial



coronal



sagittal

Reanimated destination patient

$C = 0 \text{ HU}$, $W = 1400 \text{ HU}$

Cardio-Respiratory Motion Phantom

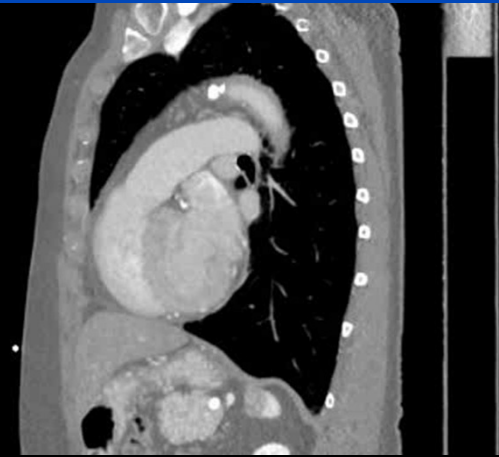
- Composition of cardiac and respiratory MVFs leads to 5D motion



axial



coronal



sagittal

Reanimated destination patient

$C = 0 \text{ HU}$, $W = 1400 \text{ HU}$

CBCT Simulations of Phantom

- The motion phantom was used to simulate rawdata corresponding to a Varian True Beam scan.
- Cardio-respiratory motion was simulated by forward projecting the motion phantom according to each projection's cardiac and respiratory phase.
- Phase-correlated Feldkamp (PCF) and artifact-specific cyclic motion compensation (acMoCo^{1,2,3}) performed for reconstruction.

¹ Brehm, Paysan, Oelhafen, Kunz, and Kachelrieß, "Self-adapting cyclic registration for motion-compensated cone-beam CT in image-guided radiation therapy," Med. Phys. 39(12), 7603-7618, 2012.

² Brehm, Paysan, Oelhafen, and Kachelrieß, "Artifact-resistant motion estimation with a patient-specific artifact model for motion-compensated cone-beam CT" Med. Phys. 40(10):101913, 2013.

³ Brehm, Sawall, Maier, and Kachelrieß, "Cardio-respiratory motion-compensated micro-CT image reconstruction using an artifact model-based motion estimation" Med. Phys. 42(4):1948-1958, 2015.

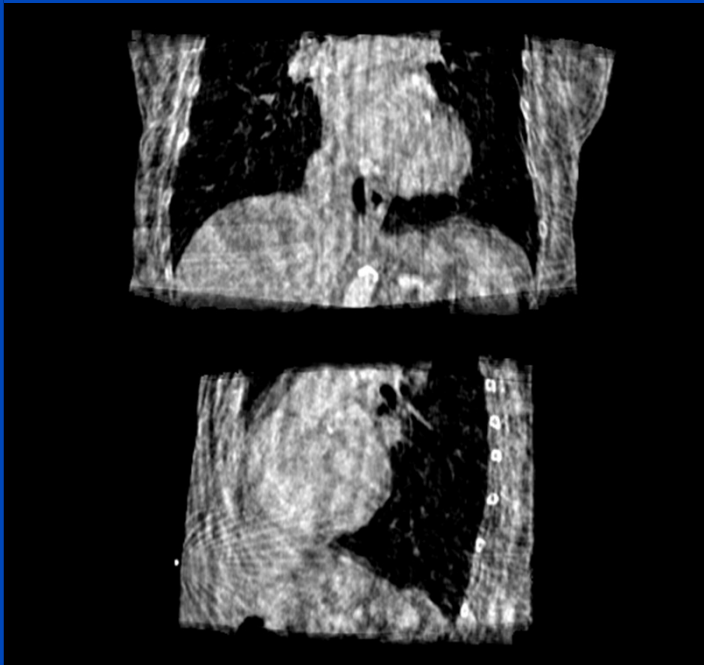
Simulated scan Parameters

Readout rate = 11 fps
Respiratory rate = 17 rpm
Heart rate = 67 bpm
Gantry rotation = 3 ° / second

acMoCo of Respiratory Motion

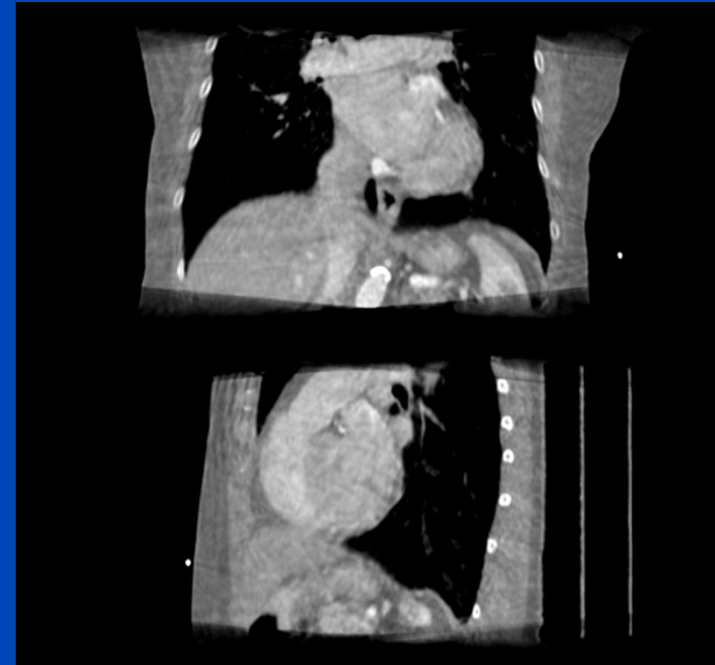
Phase-correlated FDK reconstructions (PCF)

- 20% dose usage
- significant artifacts



Motion-Compensated reconstructions (acMoCo)

- 100% dose usage
- nearly artifact-free

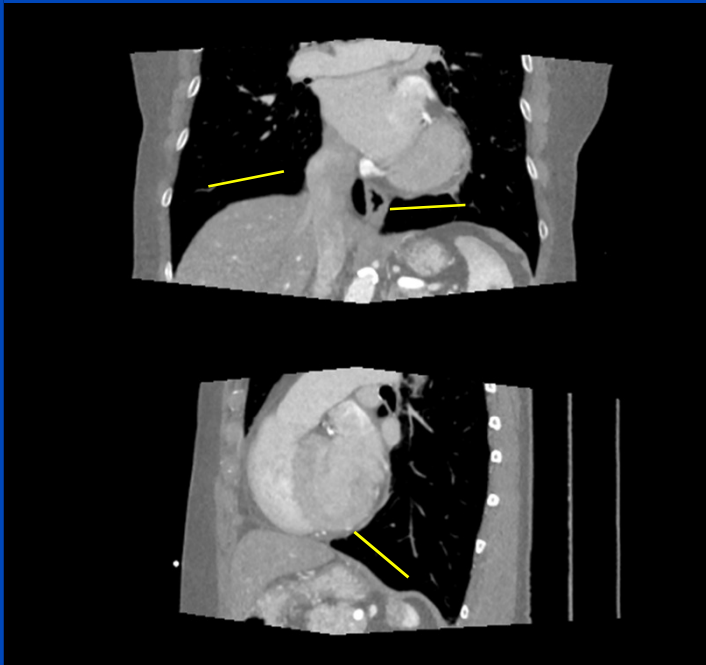


$C = 0 \text{ HU}$, $W = 1400 \text{ HU}$

Comparison of GT and acMoCo

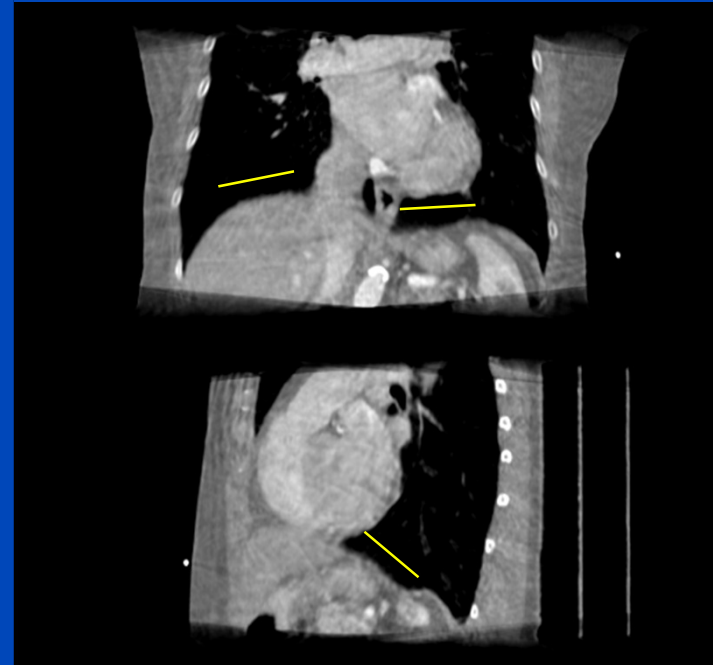
Ground truth respiratory motion

- ideal image
- no artifacts



Motion-Compensated reconstructions (acMoCo)

- 100% dose usage
- nearly artifact-free



One can detect a slight motion underestimation in the acMoCo images.

$C = 0$ HU, $W = 1400$ HU

Evaluation of MVF Deviation

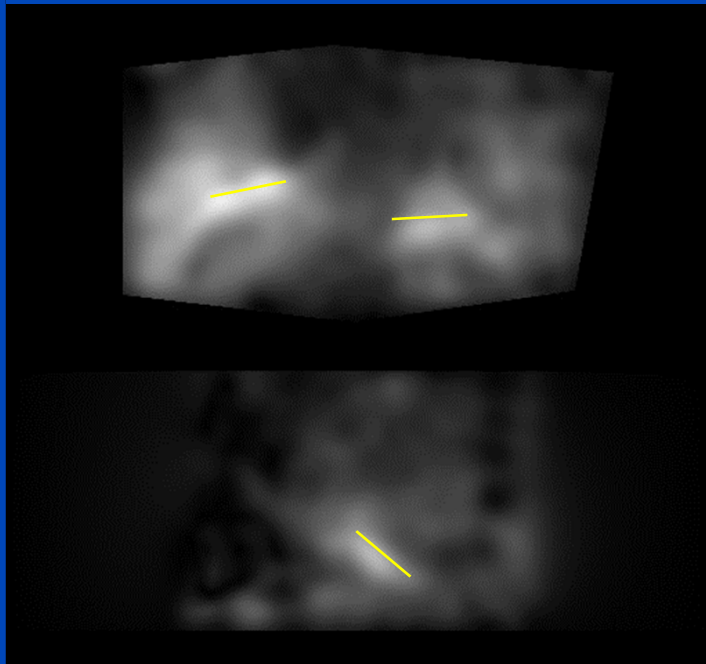
- Each ground truth voxel position $m_t^{\text{GT}}(\mathbf{r})$ is known at each time point. A direct comparison to the estimated motion $m_t^{\text{acMoCo}}(\mathbf{r})$ is performed.
- The acMoCo algorithm takes all phase-correlated images into account during motion compensation to achieve 100% dose usage.
- Hence to quantify the deviation between the estimated MVFs and the ground truth one needs to evaluate the deviation average over all phases:

$$\Delta(\mathbf{r}) = \left\| \left\langle m_t^{\text{GT}}(\mathbf{r}) - m_t^{\text{acMoCo}}(\mathbf{r}) \right\rangle_t \right\|$$

Motion Vector Field Deviation

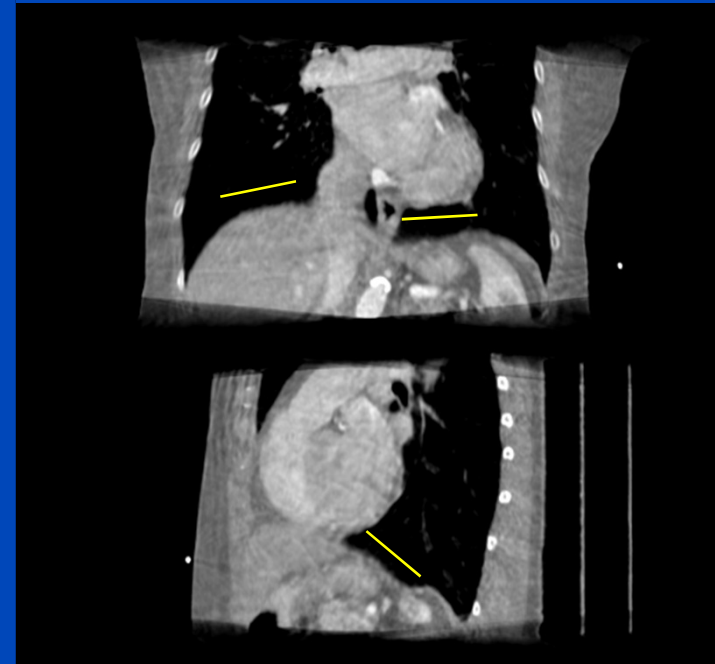
MVF
deviation

$$\Delta(\mathbf{r}) = \left\| \langle \mathbf{m}_t^{\text{GT}}(\mathbf{r}) - \mathbf{m}_t^{\text{acMoCo}}(\mathbf{r}) \rangle_t \right\|$$



Motion-compensated
reconstructions (acMoCo)

- 100% dose usage
- nearly artifact-free



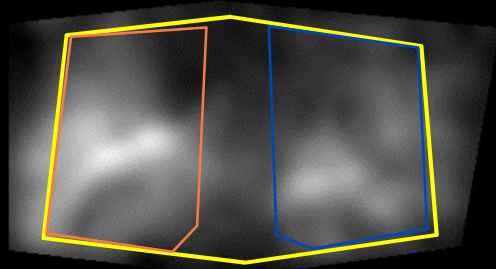
Largest deviation in maximum-amplitude phase.
Motion underestimation appears at the diaphragm.

$C = 3 \text{ mm}$, $W = 6 \text{ mm}$

$C = 0 \text{ HU}$, $W = 1400 \text{ HU}$

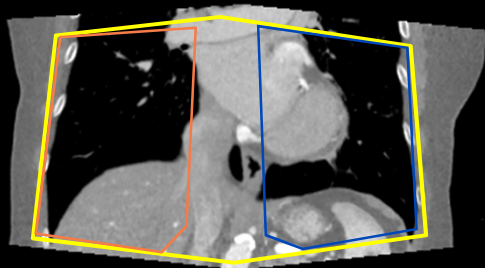
Respiratory MVF Accuracy

MVF deviation $\Delta(r)$

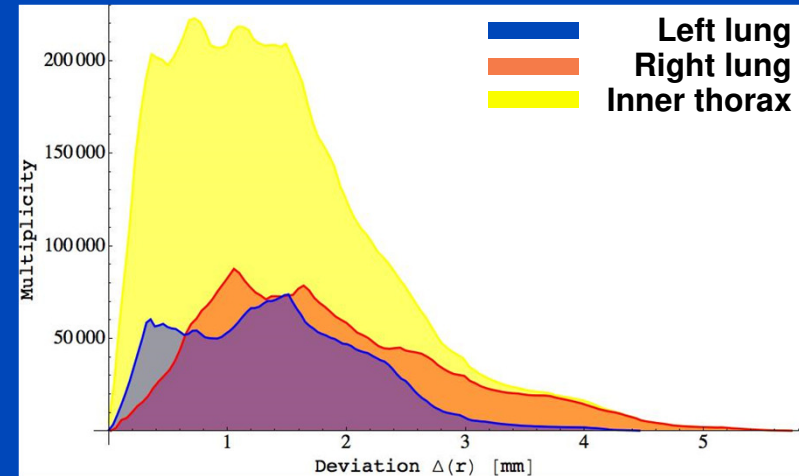


$C = 3 \text{ mm}, W = 6 \text{ mm}$

GT respiratory motion



$C = 0 \text{ HU}, W = 1400 \text{ HU}$



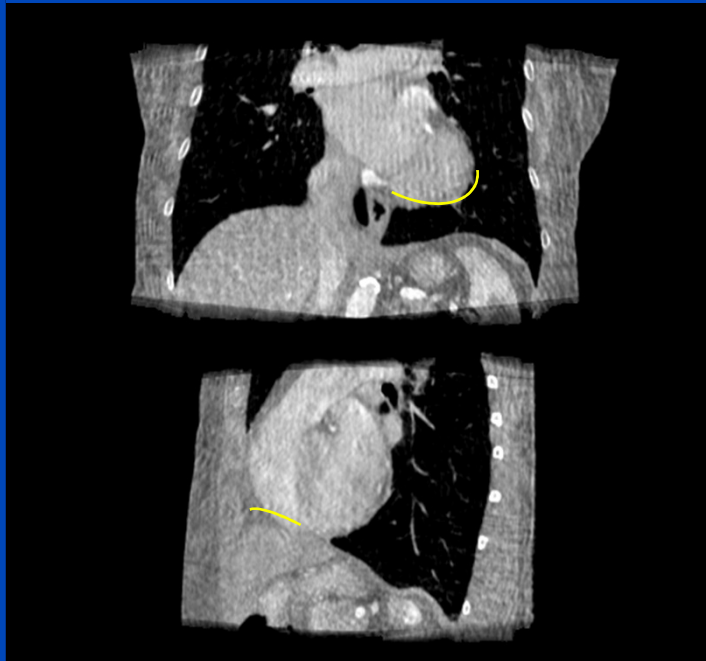
Distribution of Deviation in ROI

ROI	Deviation
Left lung	$(1.42 \pm 0.77) \text{ mm}$
Right lung	$(1.91 \pm 1.02) \text{ mm}$
Inner thorax	$(1.46 \pm 0.92) \text{ mm}$

acMoCo of Cardiac Motion

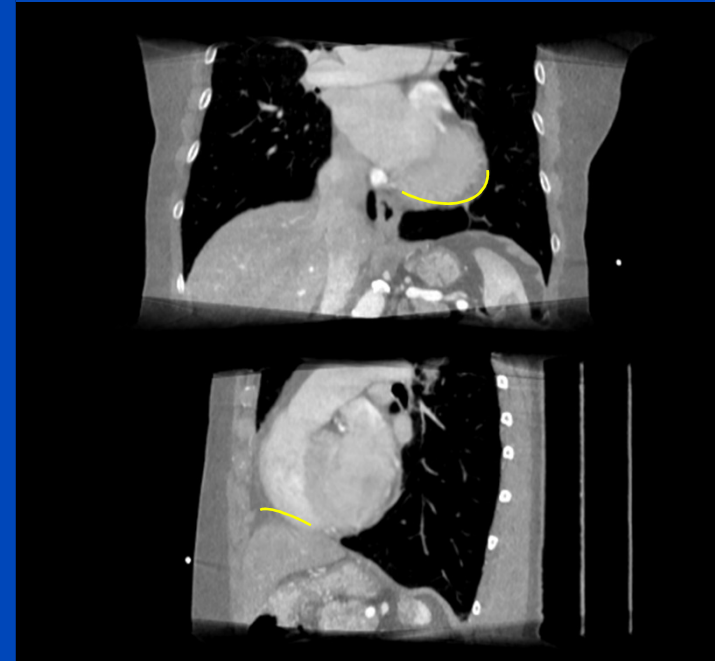
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Motion-compensated reconstructions (acMoCo)

- 100% dose usage
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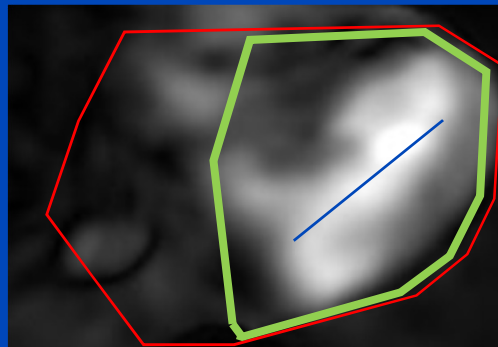


One can detect a slight motion underestimation in the acMoCo images.

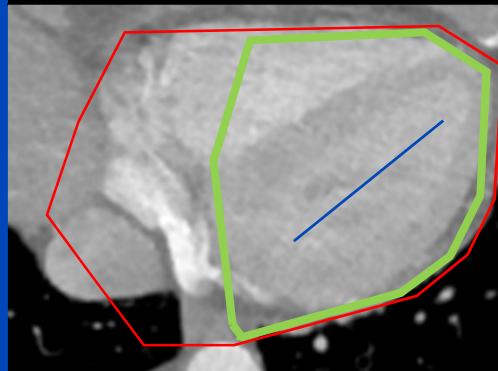
$C = 0 \text{ HU}$, $W = 1400 \text{ HU}$

Cardiac MVF Accuracy

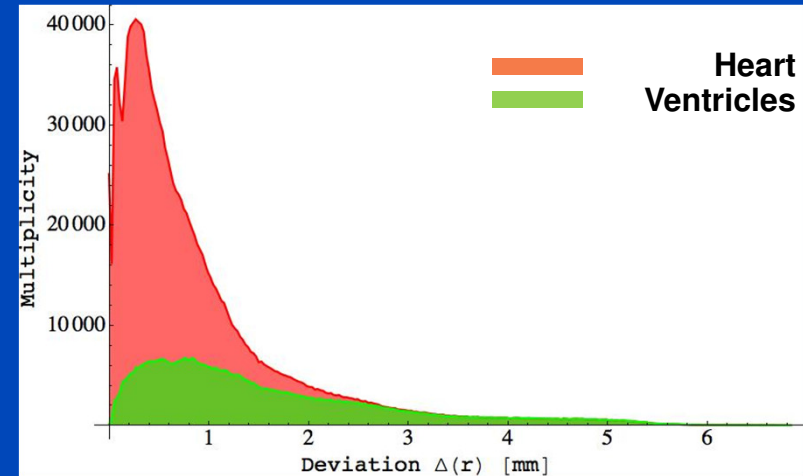
MVF deviation $\Delta(r)$



$C = 3 \text{ mm}, W = 6 \text{ mm}$



GT cardiac Motion



Distribution of Deviation in ROI

ROI	Deviation
Heart	$(0.92 \pm 0.95) \text{ mm}$
Ventricles	$(1.60 \pm 1.24) \text{ mm}$

$C = 0 \text{ HU}, W = 1400 \text{ HU}$

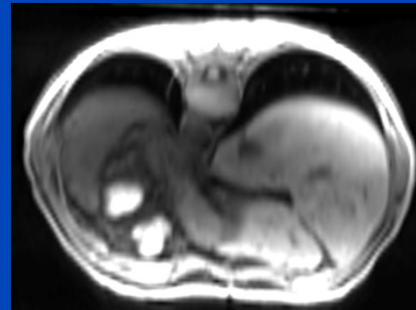
Conclusion

- Successfully simulated a 5D cardiorespiratory motion phantom on patient data. (A careful regularization of the anatomy map is needed for a reasonable motion transfer.)
- Evaluation of the acMoCo algorithm shows an accuracy of about 1.5 mm.
- Motion transfer also works between different modalities:

4D CT



Animated 3D MR



Thank You!

This presentation will soon be available at www.dkfz.de/ct.

Job opportunities through DKFZ's international PhD or Postdoctoral Fellowship programs (www.dkfz.de), or directly through Marc Kachelriess (marc.kachelriess@dkfz.de).

Parts of the reconstruction software were provided by RayConStruct[®] GmbH, Nürnberg, Germany.