

# Motion Vector Field Upsampling for Precise Respiratory Motion Compensation with Cone-Beam CT of the Thorax Region

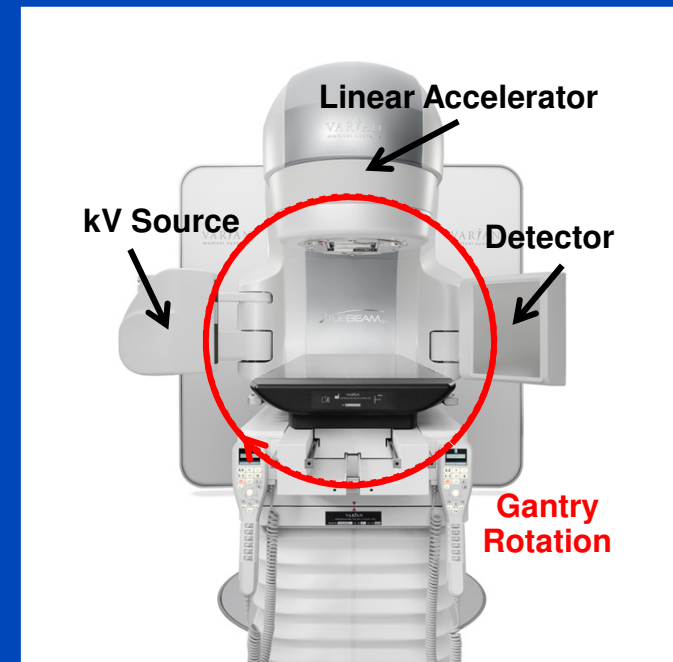
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# Slowly Rotating CBCT Devices

- Image-guided radiation therapy (IGRT)
  - Cone-beam CT (CBCT) imaging unit mounted on gantry of a LINAC treatment system
  - Accurate information about patient motion required for radiation therapy
- Slow gantry rotation speed of  $6^\circ$  per second ( $60 \text{ s}/360^\circ$ )
  - Much slower than clinical CT devices
- Breathing about 10 to 30 respiration cycles per minute (and thus per scan)
- Heartbeat about 50 to 80 beats per minute



Motion blurring in standard 3D reconstruction



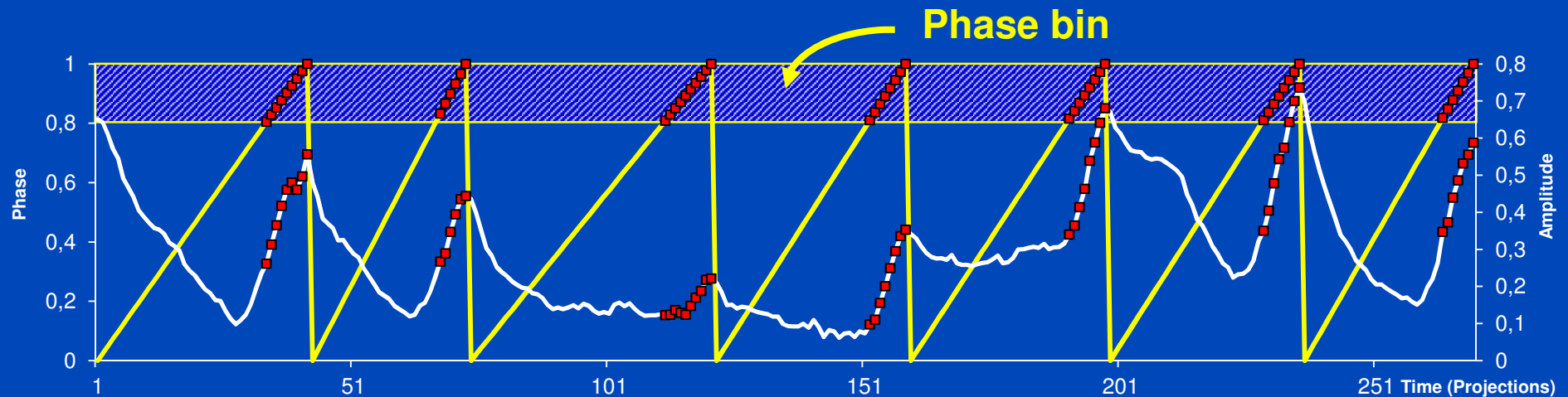
5D\* Motion compensation removes almost all motion blurring

**Account for patient motion!**

# Aims

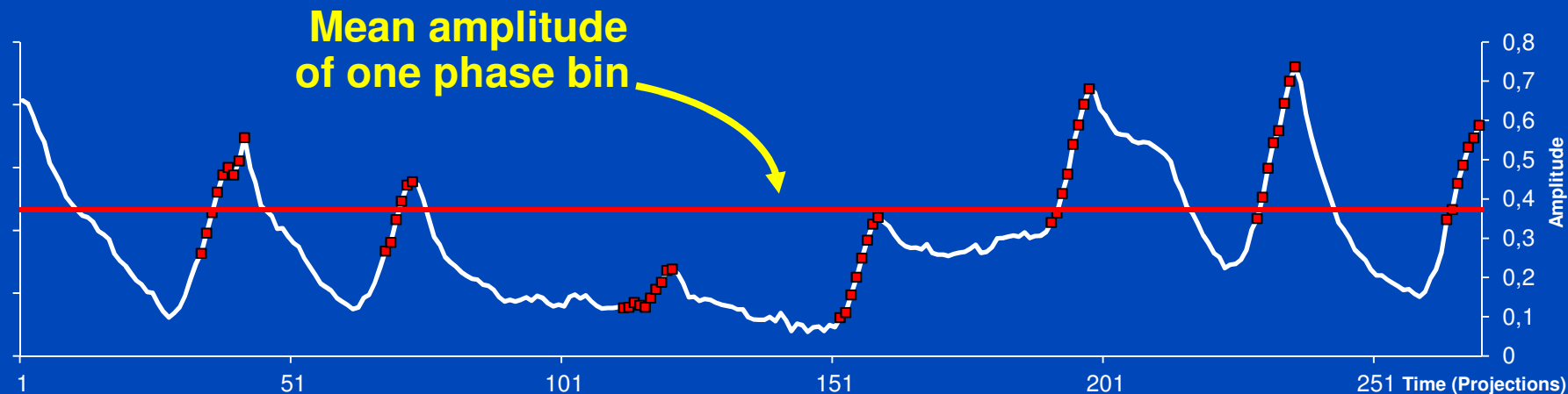
- To provide high fidelity motion-compensated (MoCo) respiratory- or cardiac-correlated volumes from CBCT.
- To further increase the temporal resolution by motion vector field (MVF) resampling.
- Use cases for MoCo (in the field of radiation therapy):
  - Accurate patient positioning
  - Reduce irradiation of the heart (organ at risk)
  - Treatment verification
  - Online treatment adaption
  - ...

# Step 1: Phase Gating



- The white curve shows a respiratory amplitude signal (external monitor)
- **The yellow curve** shows the dedicated phase signal (modulo 1)
- **The red squares** are phase-gated projections (phase and amplitude ordinates)
- Phase gating ensures a nearly uniform projection distribution for all phases
- Phase-gated projections may have a strong variation in their respiratory amplitude. This introduces motion blurring even with perfect MVFs.

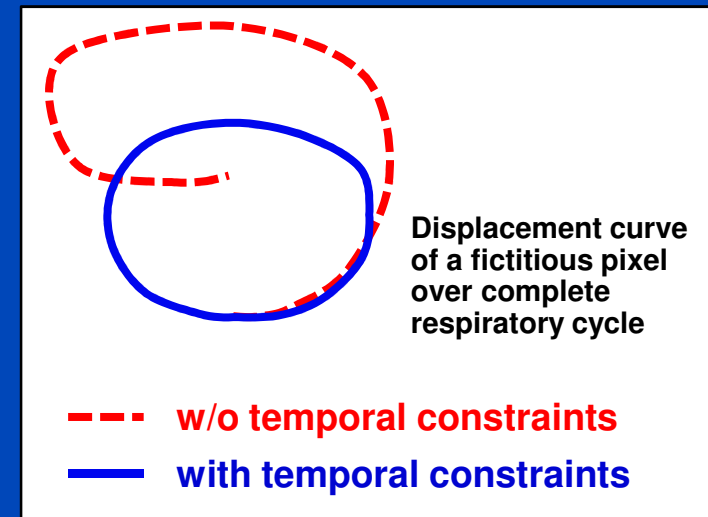
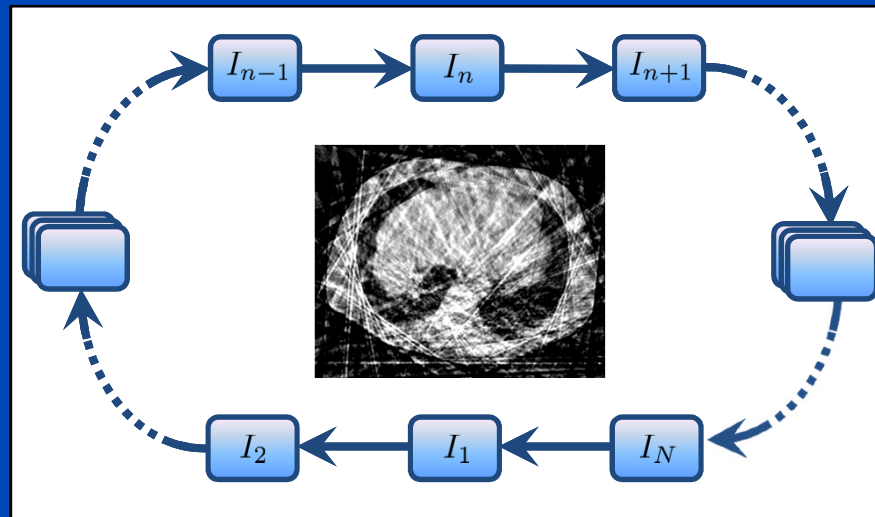
# Mean Amplitude of Phase Bins



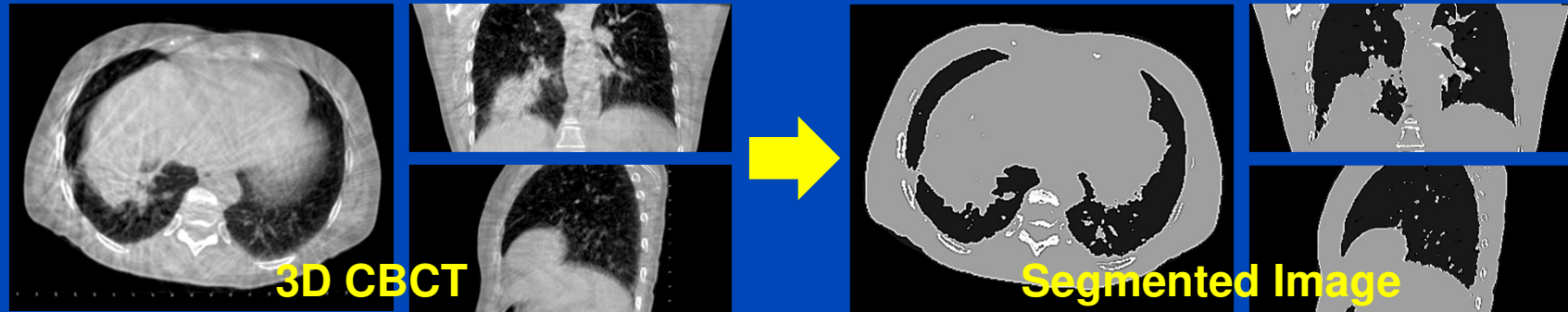
- The white curve shows a respiratory amplitude signal
- **The red line** represents the average amplitude of all projections in this phase
- Motion estimation is done between adjacent phase bins
- Pragmatic assumption: The MVFs describe the deformation between the mean amplitude of adjacent phase bins

# Step 2: a) Motion Estimation with Cyclic Regularization (cMoCo)

- Motion estimation only between adjacent phases
- Incorporate additional knowledge
  - A priori knowledge of quasi periodic breathing pattern
  - Non-cyclic motion is penalized
  - Error propagation due to concatenation is reduced



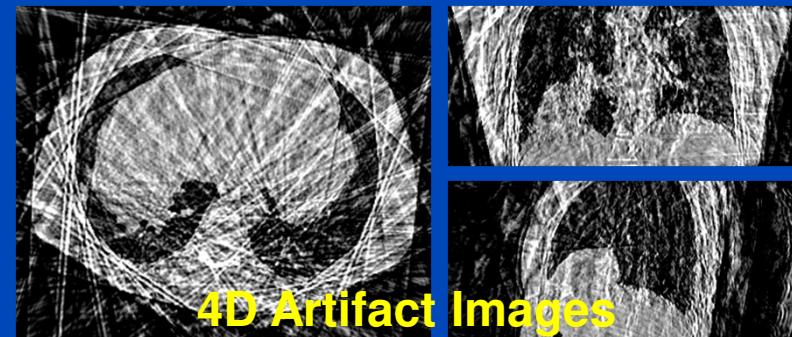
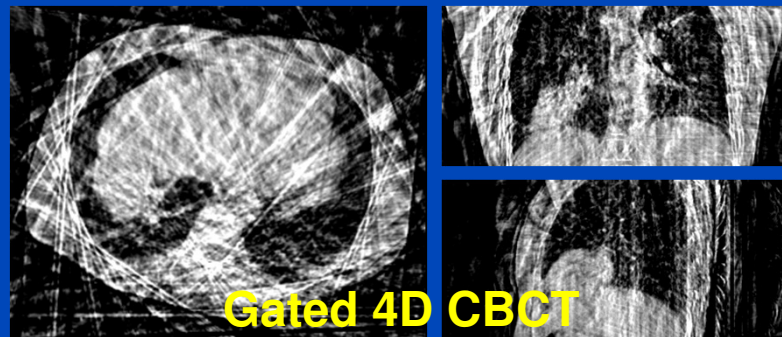
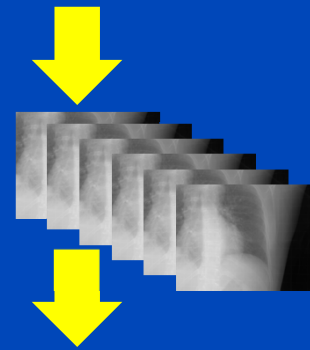
# Step 2: b) Motion Estimation with Artifact-Model-Based Regularization (aMoCo)



Measured data:

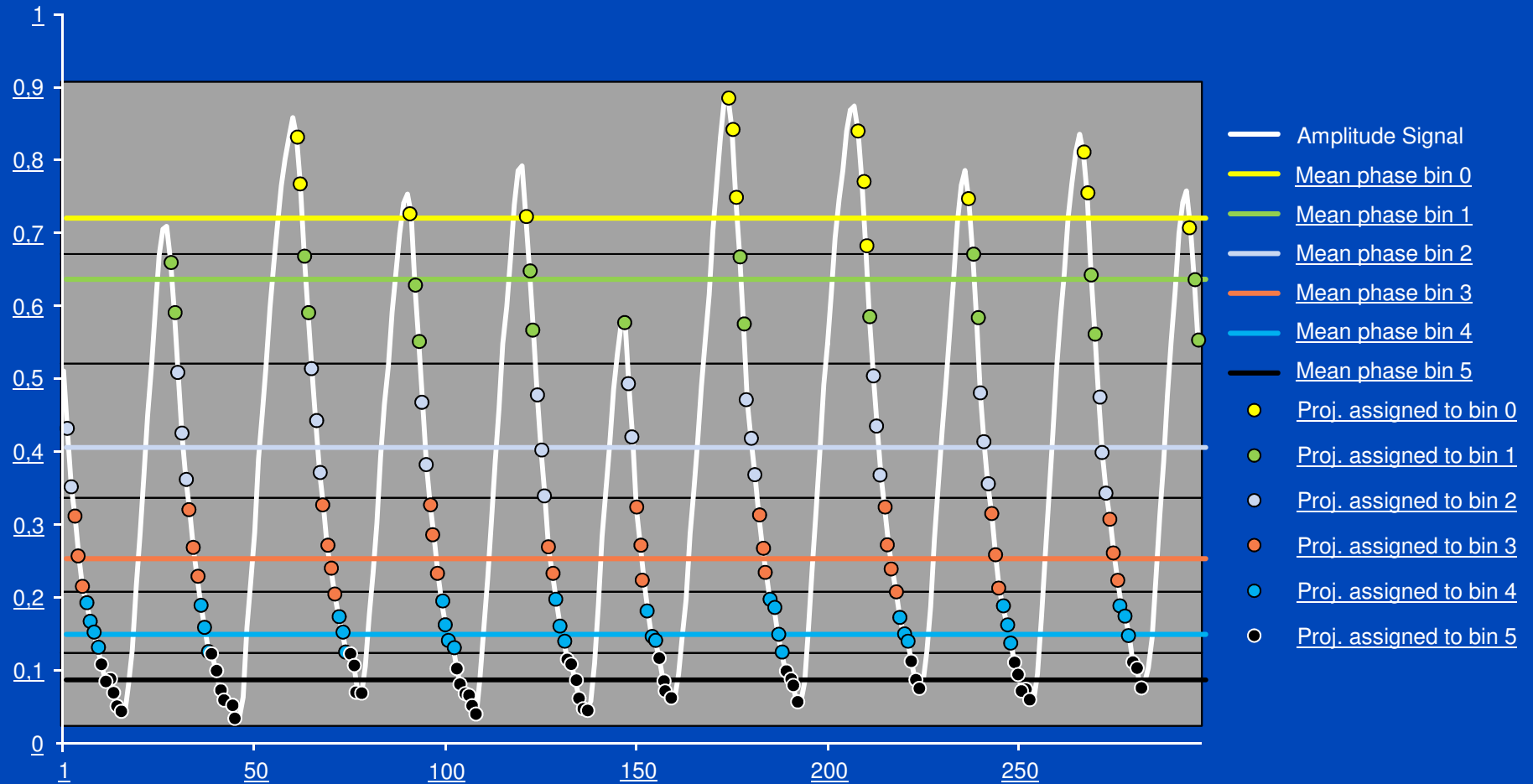


Virtual rawdata:



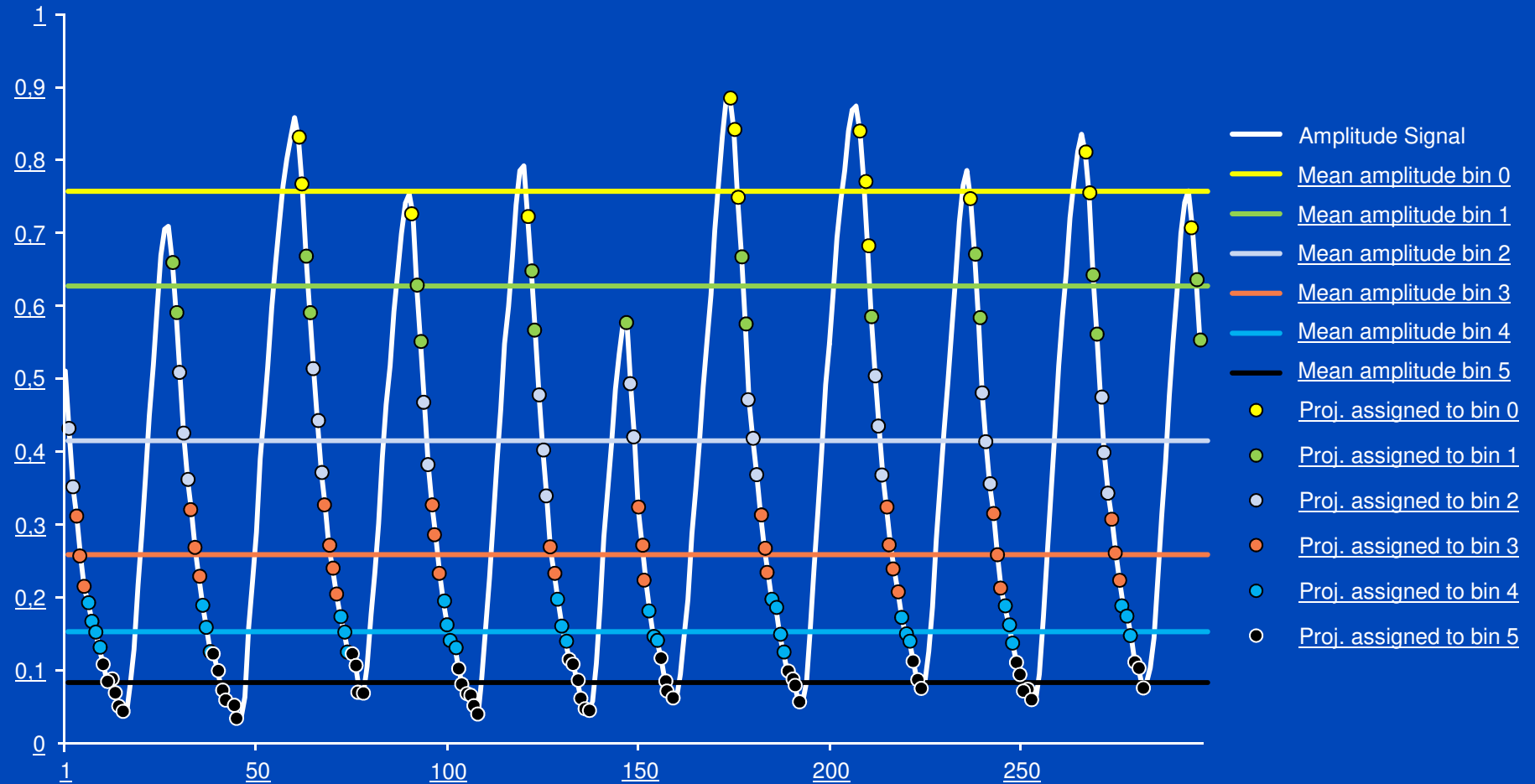
# Step 3: Defining the Amplitude Bins

(exhale period shown,  $R=10$ ,  $K=1$ )

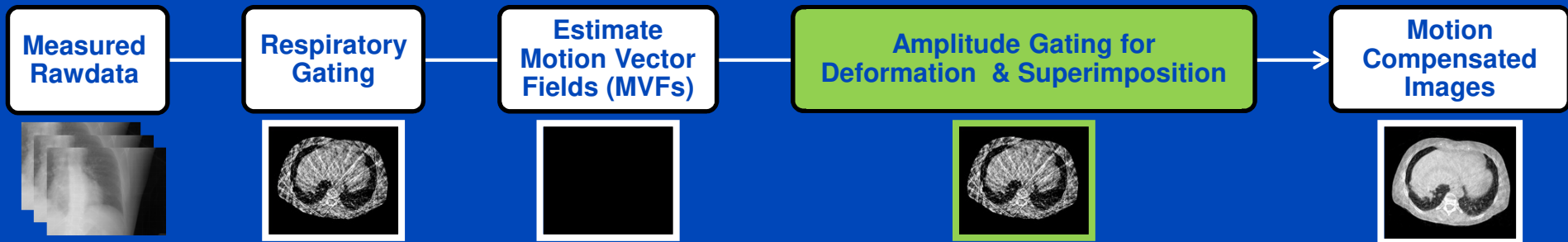




# Step 4: Recalculation of the Mean Amplitudes

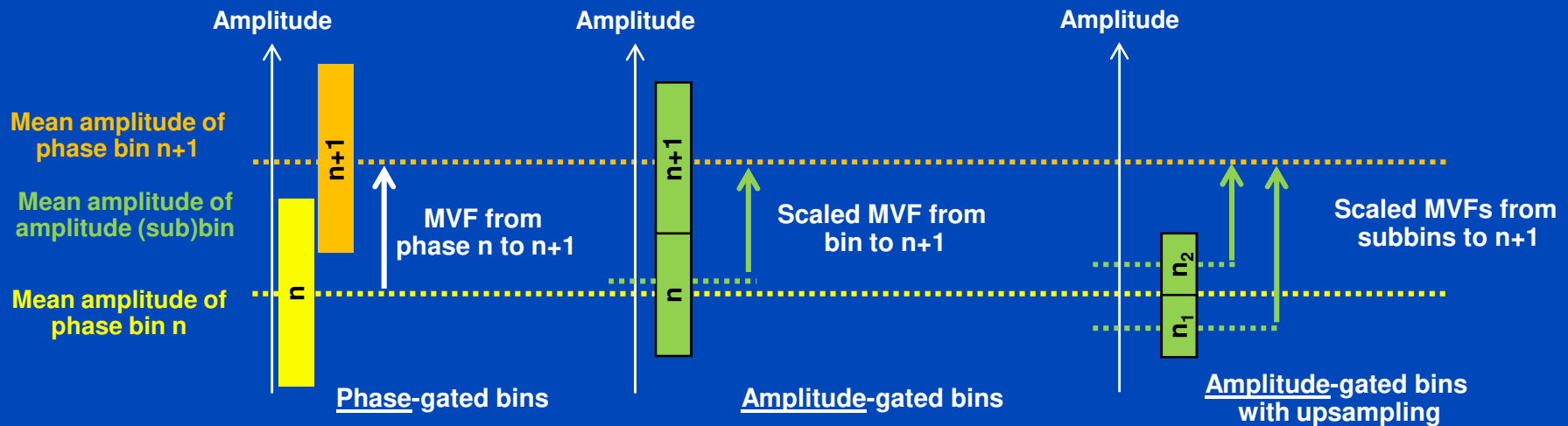


# Switching From Phase to Amplitude Binning



**Phase gating**  
for motion estimation

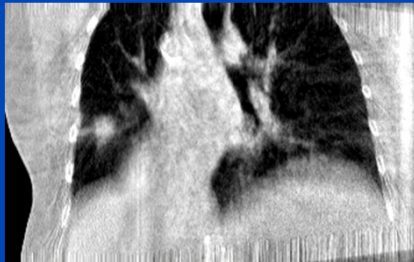
**Amplitude gating**  
for deformation & superimposition



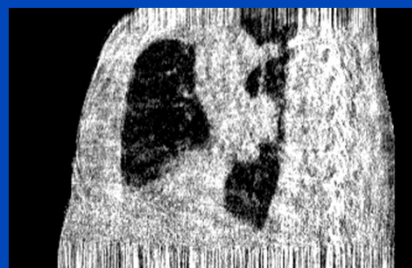
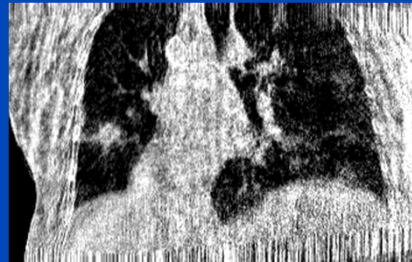
# Patient Data

Motion Compensation R=10, 20% Bin Width  
Scan Velocity 2 °/s with 7 fps, 13 rpm

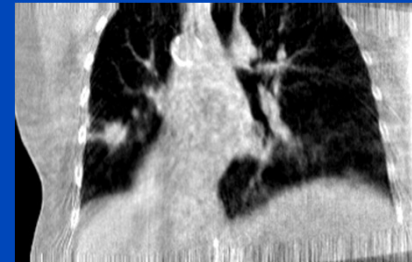
3D FDK



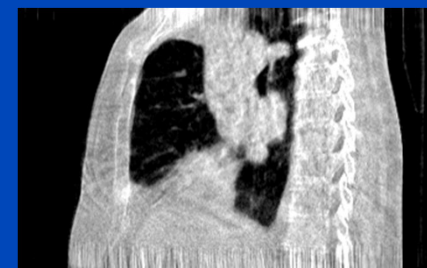
PCF  
R=10



acMoCo  
R=10



acMoCo  
R=10, MVF Resampling



# Summary

- MVF estimation and thus MoCo image reconstruction can be significantly improved by MVF phase-to-amplitude resampling.
- Motion blurring was reduced in all motion bins.

# Thank You!

- This study was supported by Varian Medical Systems.
- This presentation will soon be available at [www.dkfz.de/ct](http://www.dkfz.de/ct).
- Job opportunities through DKFZ's international PhD or Postdoctoral Fellowship programs ([www.dkfz.de](http://www.dkfz.de)), or directly through Marc Kachelrieß ([marc.kachelriess@dkfz.de](mailto:marc.kachelriess@dkfz.de)).
- Parts of the reconstruction software were provided by RayConStruct<sup>®</sup> GmbH, Nürnberg, Germany.