

# Performance of Today's Dual Energy CT and Future Multi Energy CT in Virtual Non Contrast Imaging and in Iodine Quantification

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X-Ray Imaging and Computed Tomography, E025

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# DECT Technology

- **In the clinic:**

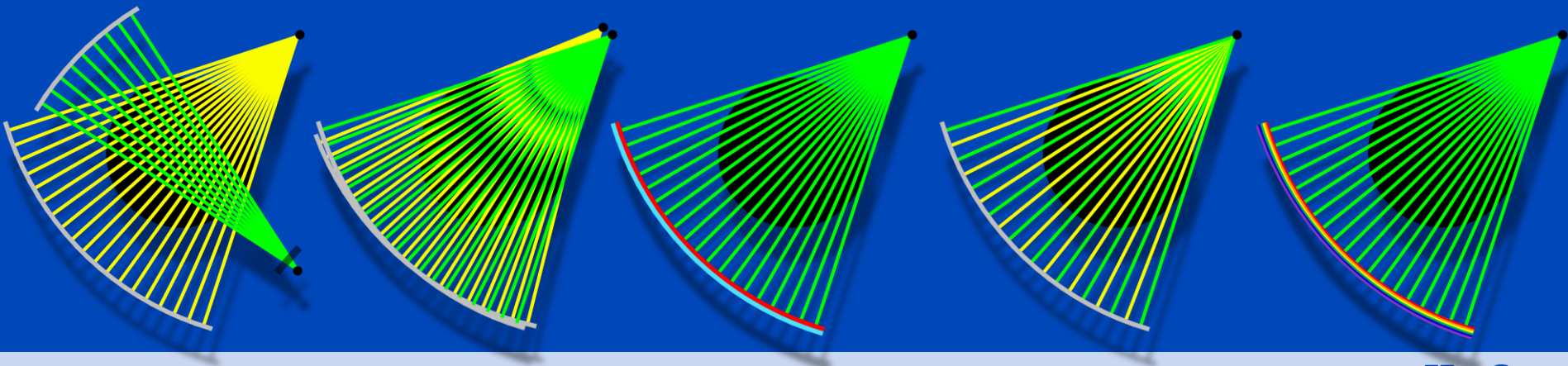
- Multiple scans at different spectra
- Dual source CT (DSCT), generations 2, and 3
- Fast tube voltage switching
- Dual layer sandwich detectors
- Split filter

mid-range  
high-end  
high-end  
high-end  
mid-range

- **First prototypes:**

- Photon counting detectors (two or more energy bins)

high-end



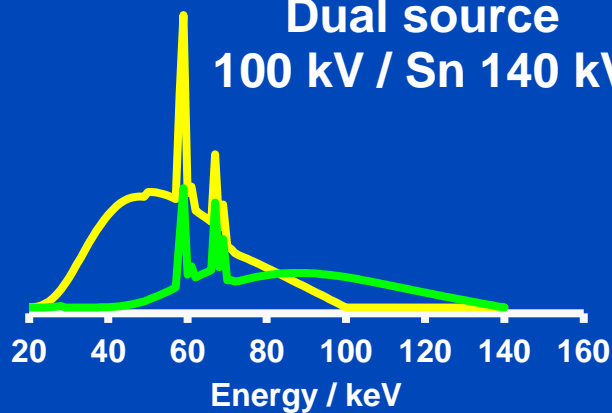
# Simulations

- Study typical dual energy CT (DECT) application:
  - Material decomposition: virtual non contrast (VNC) and iodine image
- Comparison of:
  - Different DECT techniques with energy integrating (EI) detectors
  - Energy-selective photon counting (PC) detectors
- Statistically optimal material decomposition:
  - Constant contrast due to calibration
  - Constant patient dose in all cases (absorbed energy)
  - Noise minimization = CNRD maximization
- Based on low noise patient data set:
  - Averaged over 8 thin slices
  - Separation into water and iodine
  - Forward projection for material-specific polychromatic sinograms
- DECT image noise:
  - Approximately the same in low and high energy images
  - 100 kV / Sn 140 kV: Low / high 230 mAs / 180 mAs,  $\sigma_{\text{low}} / \sigma_{\text{high}} = 1.13$

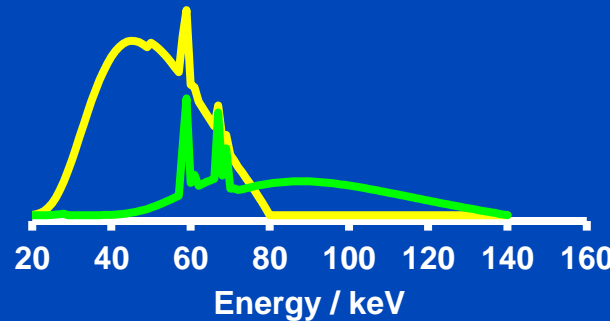


# DECT Spectra

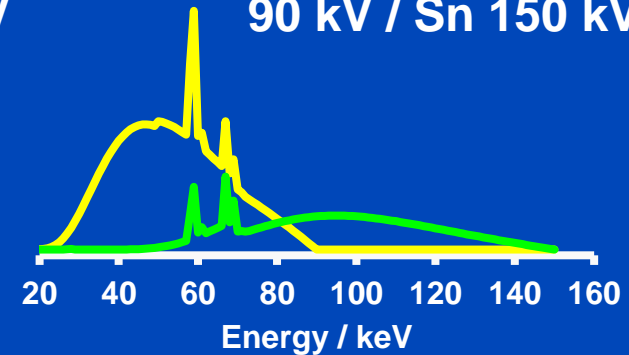
Dual source  
100 kV / Sn 140 kV



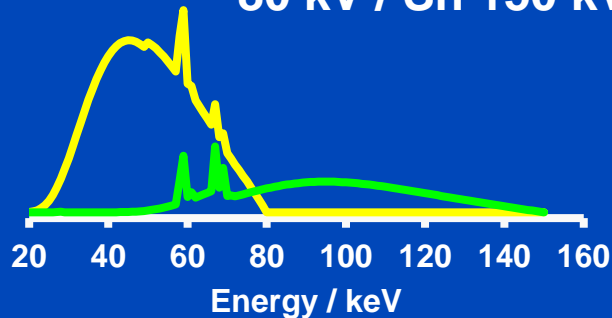
Dual source  
80 kV / Sn 140 kV



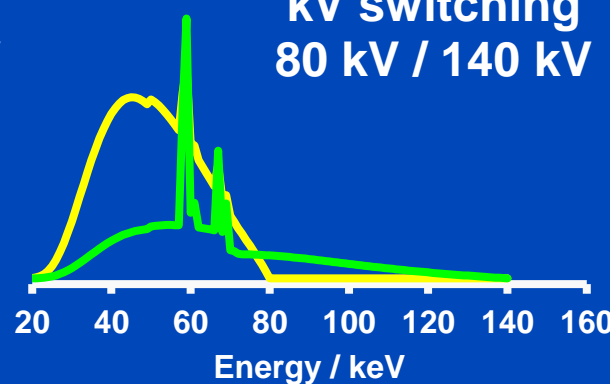
Dual source  
90 kV / Sn 150 kV



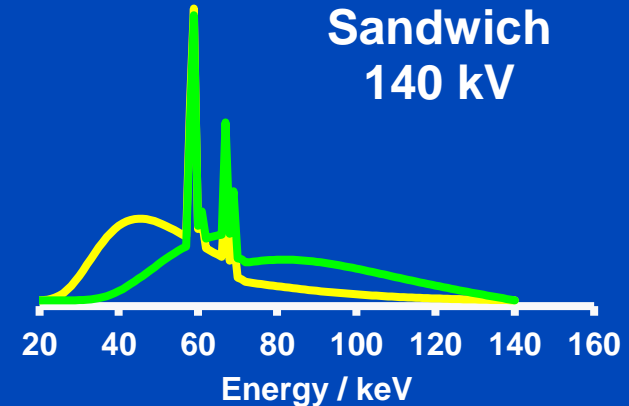
Dual source  
80 kV / Sn 150 kV



kV switching  
80 kV / 140 kV



Sandwich  
140 kV



- Overlap between low and high energy spectrum important in image-based material decomposition
- Mutual information in both spectra increase noise in image subtraction

# Results – Different DSCT Generations

2<sup>nd</sup> generation DSCT

3<sup>rd</sup> generation DSCT

DS 100 kV / Sn 140 kV

DS 80 kV / Sn 140 kV

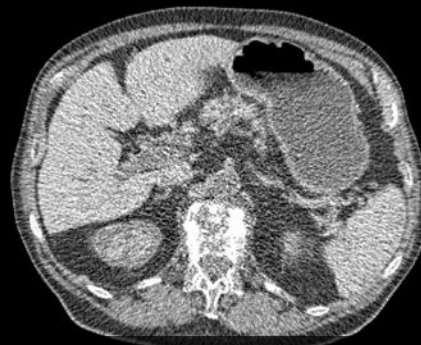
DS 90 kV / Sn 150 kV

DS 80 kV / Sn 150 kV

VNC



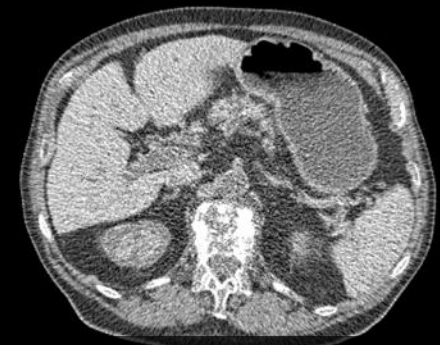
reference



-18% noise

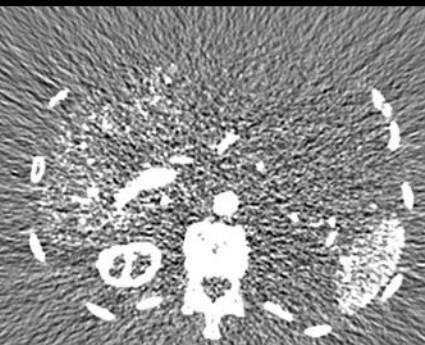


-24% noise

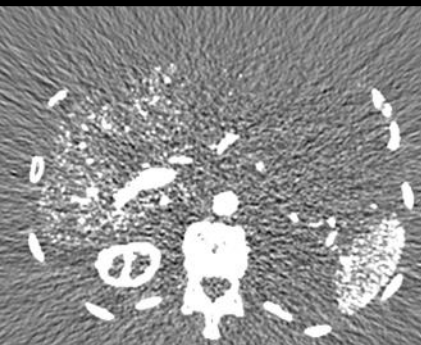


-28% noise

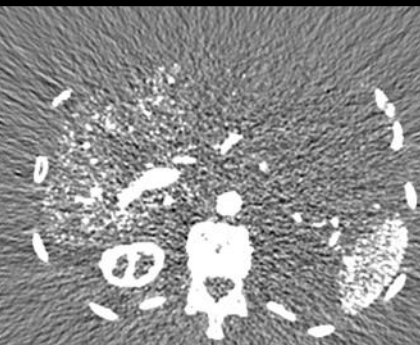
Iodine



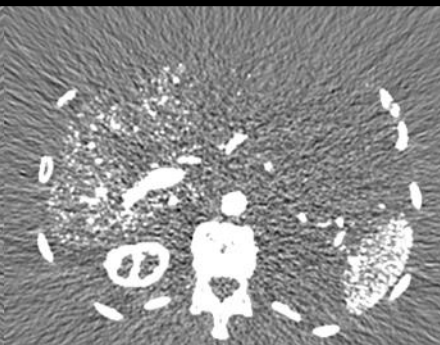
reference



-31% noise



-27% noise



-38% noise

# Results – Different DECT Techniques



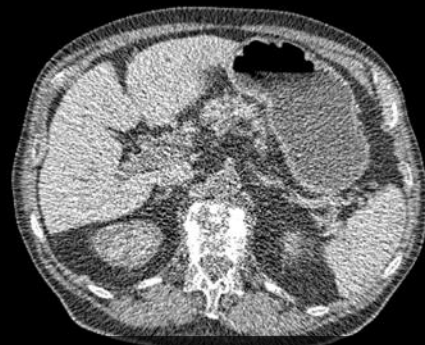
DS 100 kV / Sn 140 kV

DS 80 kV / Sn 140 kV

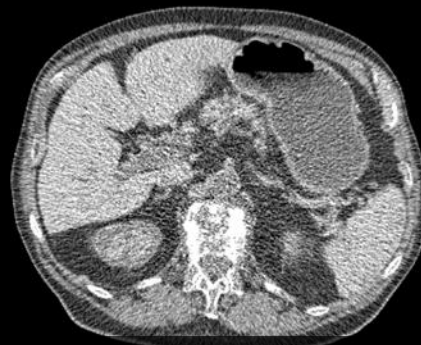
TVS 80 kV / 140 kV

Sandwich 140 kV

VNC



reference



-18% noise

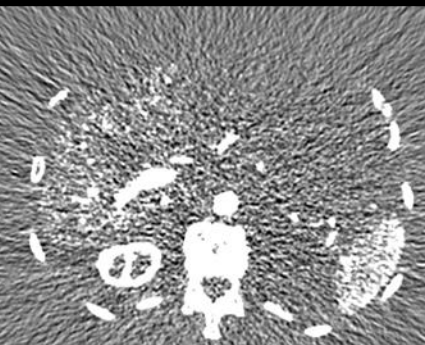


+35% noise

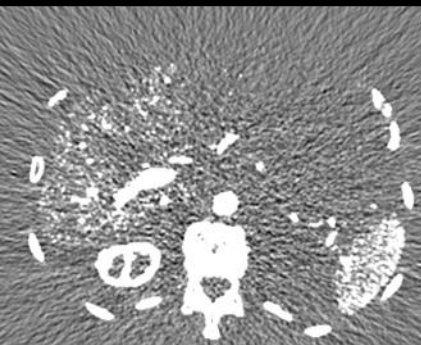


+41% noise

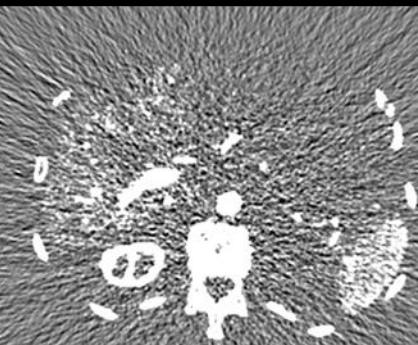
Iodine



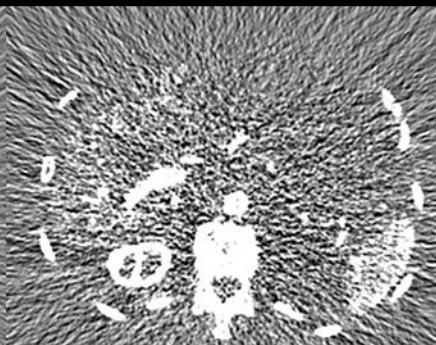
reference



-31% noise



+2% noise

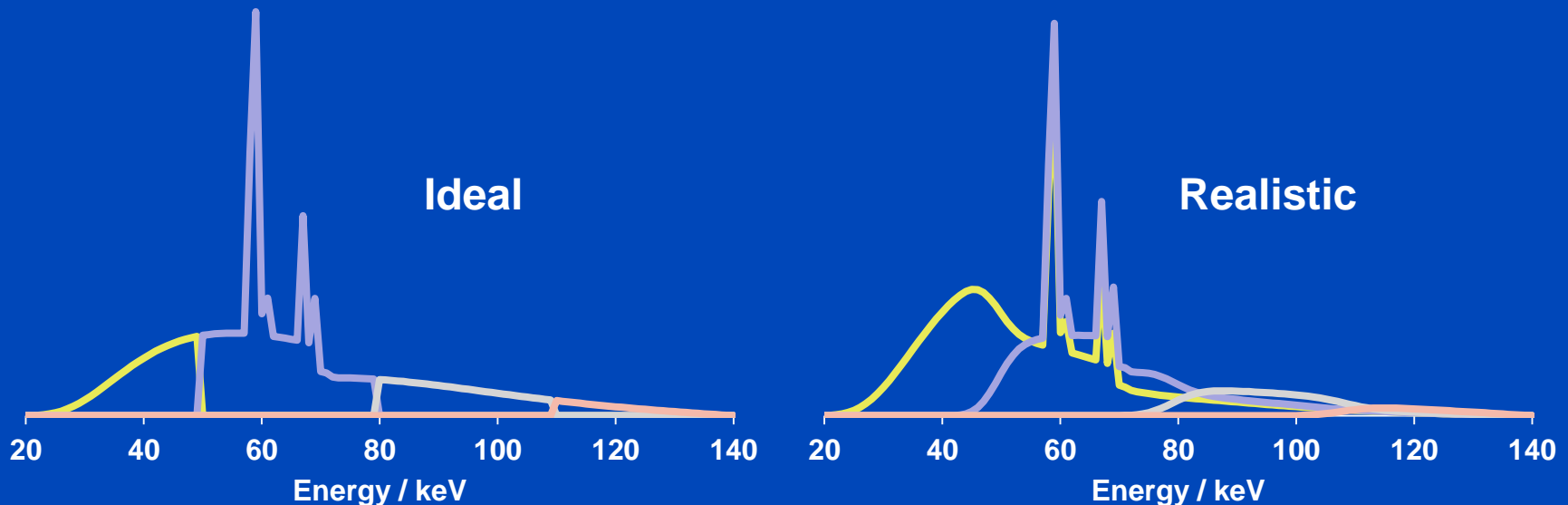


+50% noise

# MECT Simulation

- Photon counting detector
- Energy bin spectra for  $B = 4$ :

Energy bins equidistantly placed from 20 keV to 140 keV.



# Results – PC (Ideal Model)

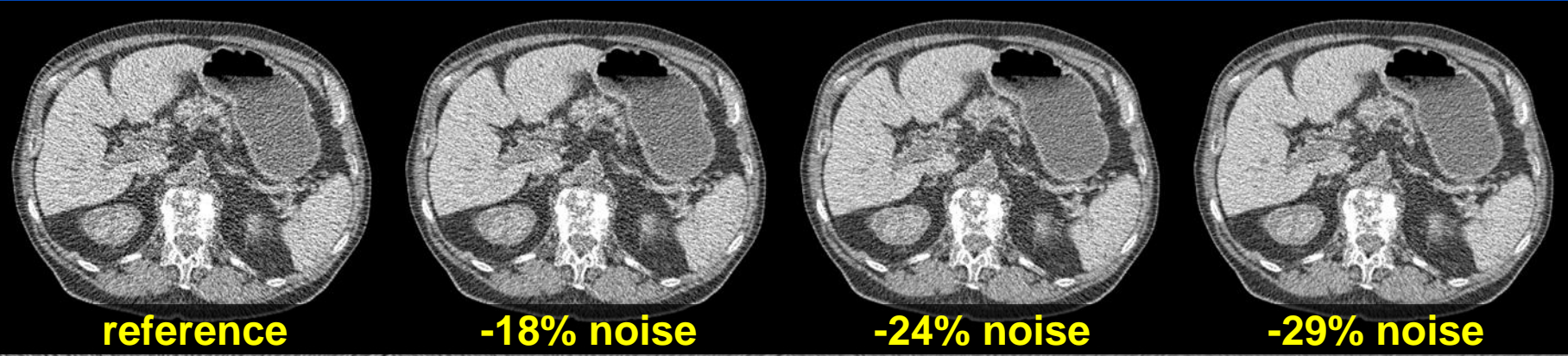
DS 100 kV / Sn 140 kV

PC 2 bins

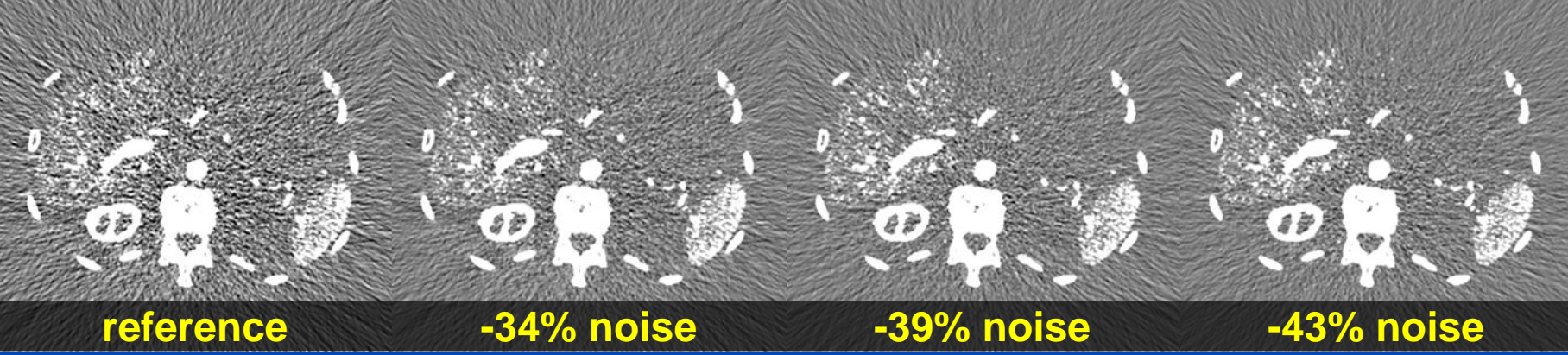
PC 4 bins

PC 8 bins

VNC



Iodine





# Results – PC (Realistic Model)

DS 100 kV / Sn 140 kV

PC 2 bins

PC 4 bins

PC 8 bins

VNC



reference



+21% noise

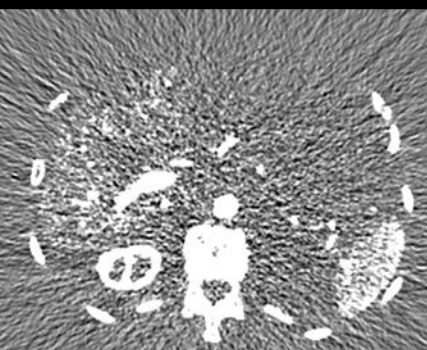


+15% noise

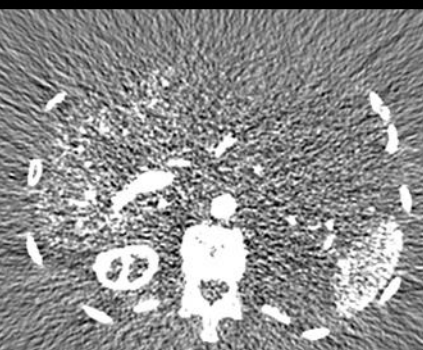


+9% noise

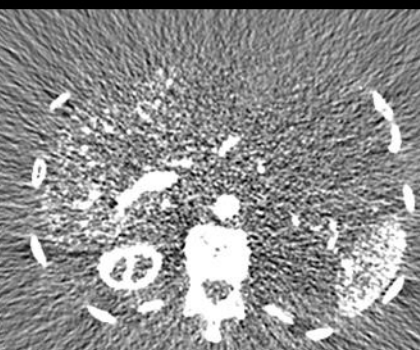
Iodine



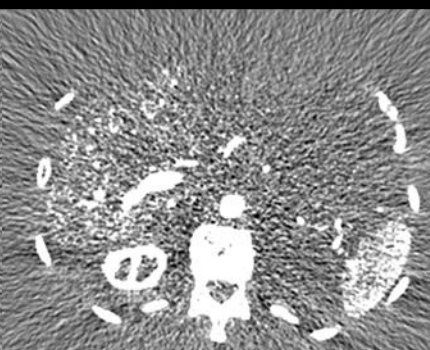
reference



+1% noise



-4% noise



-10% noise

# Overview Results

		Water-equivalent image		Iodine map	
		Noise	Dose	Noise	Dose
<b>DS 100 kV / Sn 140 kV</b>	<b>2<sup>nd</sup> g.</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>
DS 80 kV / Sn 140 kV	2 <sup>nd</sup> g.	-18%	-32%	-31%	-53%
DS 90 kV / Sn 150 kV	3 <sup>rd</sup> g.	-24%	-42%	-27%	-47%
DS 80 kV / Sn 150 kV	3 <sup>rd</sup> g.	-28%	-48%	-38%	-62%
kV switching 80 kV / 140 kV		<b>+35%</b>	<b>+83%</b>	<b>+2%</b>	<b>+4%</b>
Sandwich 140 kV		<b>+41%</b>	<b>+98%</b>	<b>+50%</b>	<b>+125%</b>
PC Ideal 140 kV 2 bins		-18%	-33%	-34%	-56%
PC Ideal 140 kV 4 bins		-24%	-43%	-39%	-62%
PC Ideal 140 kV 8 bins		-29%	-49%	-43%	-68%
PC Realistic 140 kV 2 bins		<b>+21%</b>	<b>+46%</b>	<b>+1%</b>	<b>+2%</b>
PC Realistic 140 kV 4 bins		<b>+15%</b>	<b>+32%</b>	-4%	-8%
PC Realistic 140 kV 8 bins		<b>+9%</b>	<b>+18%</b>	-10%	-19%

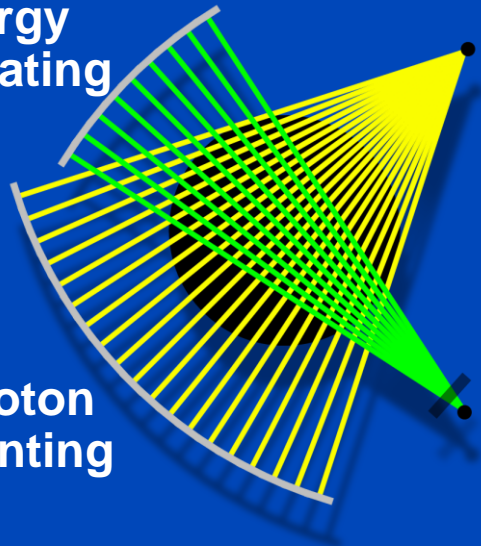
# Overview Results

		Water-equivalent image		Iodine map	
		Noise	Dose	Noise	Dose
DS 100 kV / Sn 140 kV	2 <sup>nd</sup> g.	+31%	+71%	+38%	+90%
DS 80 kV / Sn 140 kV	2 <sup>nd</sup> g.	+8%	+16%	-6%	-11%
<b>DS 90 kV / Sn 150 kV</b>	<b>3<sup>rd</sup> g.</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>
DS 80 kV / Sn 150 kV	3 <sup>rd</sup> g.	-6%	-11%	-15%	-28%
kV switching 80 kV / 140 kV		+77%	+213%	+40%	+97%
Sandwich 140 kV		+84%	+239%	+107%	+327%
PC Ideal 140 kV 2 bins		+7%	+15%	-9%	-17%
PC Ideal 140 kV 4 bins		-1%	-2%	-15%	-29%
PC Ideal 140 kV 8 bins		-7%	-13%	-22%	-39%
PC Realistic 140 kV 2 bins		+58%	+149%	+39%	+95%
PC Realistic 140 kV 4 bins		+50%	+126%	+32%	+75%
PC Realistic 140 kV 8 bins		+42%	+101%	+24%	+54%

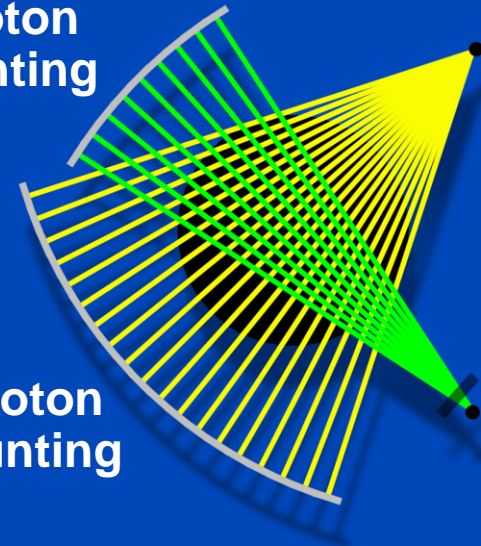
# PC/EI and PC/PC DSCT Concepts

- Improve PC detector performance using DSCT
- Replace low spectrum EI detector by PC detector
- Replace both EI detectors by PC detectors

Energy  
integrating



Photon  
counting



# Results – PC/EI (Realistic PC Model)

PC 100 kV / EI Sn 140 kV

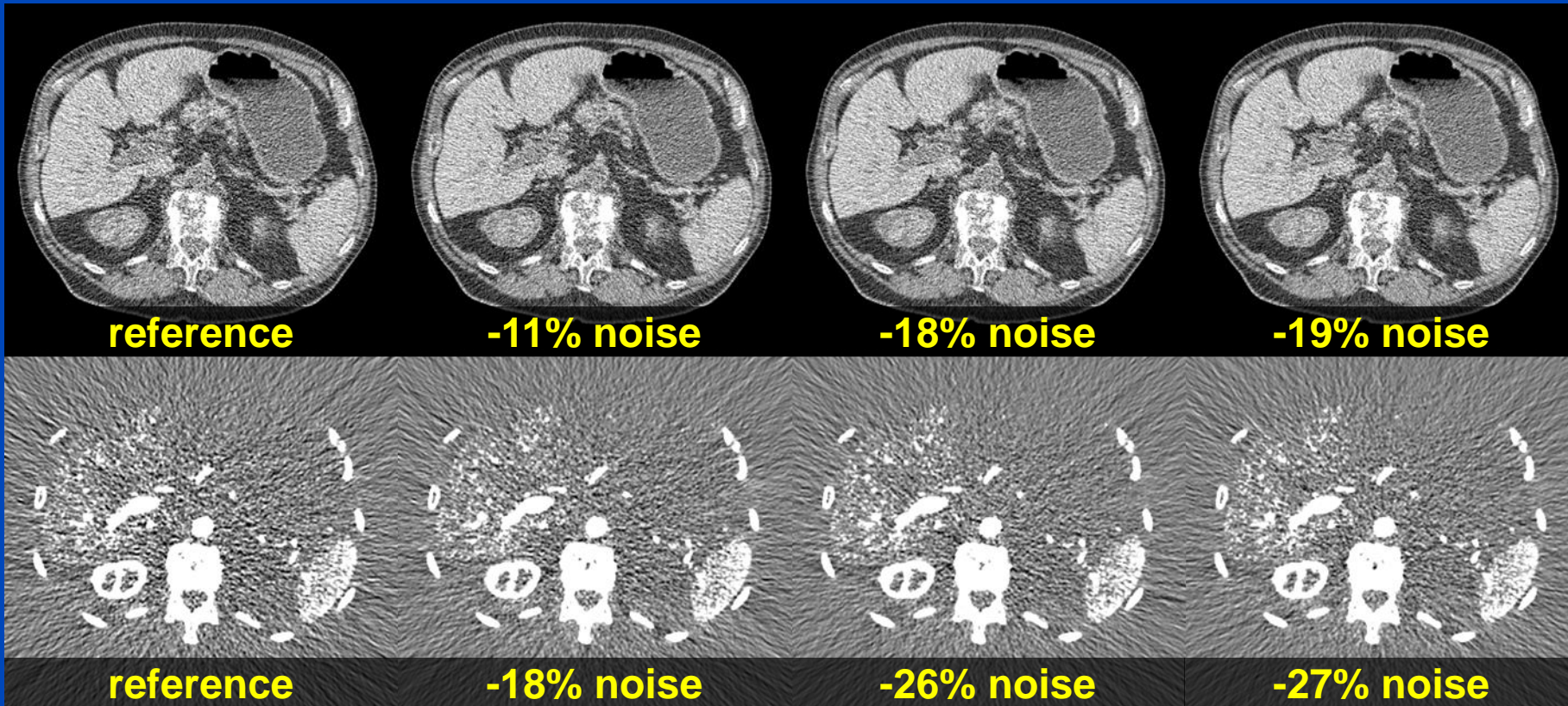
DS 100 kV / Sn 140 kV

PC 1 bin

PC 2 bins

PC 4 bins

VNC



Iodine

# Results – PC/PC (Realistic PC Model)

PC 100 kV / PC Sn 140 kV

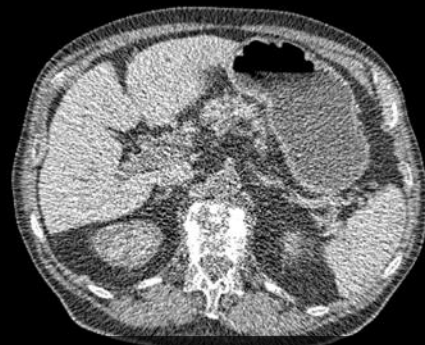
DS 100 kV / Sn 140 kV

PC 1 bin

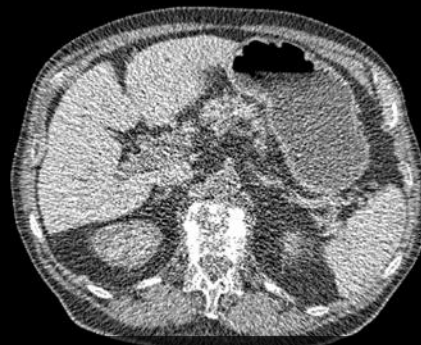
PC 2 bins

PC 4 bins

VNC



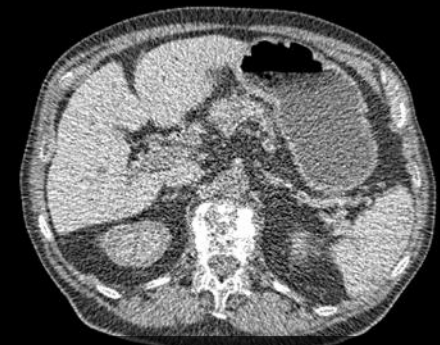
reference



+10% noise

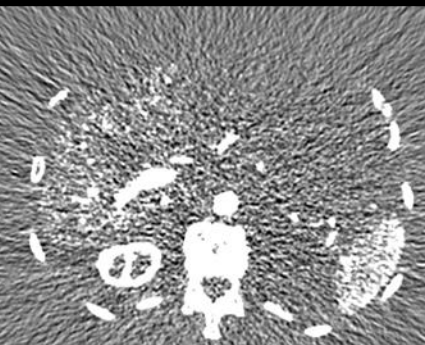


-8% noise

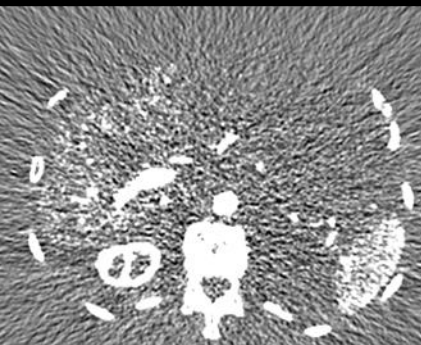


-10% noise

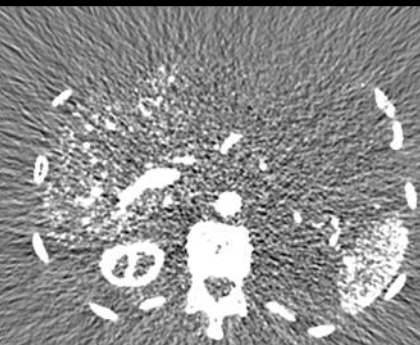
Iodine



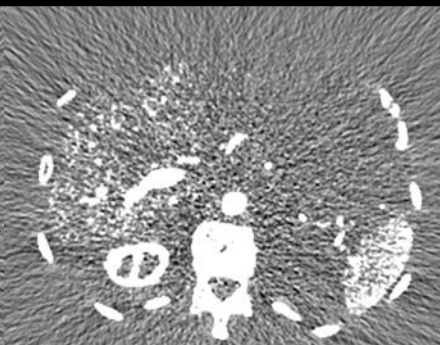
reference



-3% noise



-21% noise



-22% noise

# Overview Results

	Water-equivalent image		Iodine map	
	Noise	Dose	Noise	Dose
<b>DS 100 kV / Sn 140 kV</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>
DS 80 kV / Sn 140 kV	-18%	-32%	-31%	-53%
DS 90 kV / Sn 150 kV	-24%	-42%	-27%	-47%
DS 80 kV / Sn 150 kV	-28%	-48%	-38%	-62%
kV switching 80 kV / 140 kV	+35%	+83%	+2%	+4%
Sandwich 140 kV	+41%	+98%	+50%	+125%
PC Ideal 140 kV 2 bins	-18%	-33%	-34%	-56%
PC Ideal 140 kV 4 bins	-24%	-43%	-39%	-62%
PC Ideal 140 kV 8 bins	-29%	-49%	-43%	-68%
PC Realistic 140 kV 2 bins	+21%	+46%	+1%	+2%
PC Realistic 140 kV 4 bins	+15%	+32%	-4%	-8%
PC Realistic 140 kV 8 bins	+9%	+18%	-10%	-19%
PC 100 kV / EI Sn 140 kV 1 bin	-11%	-20%	-18%	-33%
PC 100 kV / EI Sn 140 kV 2 bins	-18%	-33%	-26%	-45%
PC 100 kV / EI Sn 140 kV 4 bins	-19%	-35%	-27%	-47%
PC 100 kV / PC Sn 140 kV 1 bin	+10%	+21%	-3%	-6%
PC 100 kV / PC Sn 140 kV 2 bins	-8%	-16%	-21%	-38%
PC 100 kV / PC Sn 140 kV 4 bins	-10%	-18%	-22%	-40%

# Overview Results

	Water-equivalent image		Iodine map	
	Noise	Dose	Noise	Dose
DS 100 kV / Sn 140 kV	+31%	+71%	+38%	+90%
DS 80 kV / Sn 140 kV	+8%	+16%	-6%	-11%
<b>DS 90 kV / Sn 150 kV</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>	<b>0%</b>
DS 80 kV / Sn 150 kV	-6%	-11%	-15%	-28%
kV switching 80 kV / 140 kV	+77%	+213%	+40%	+97%
Sandwich 140 kV	+84%	+239%	+107%	+327%
PC Ideal 140 kV 2 bins	+7%	+15%	-9%	-17%
PC Ideal 140 kV 4 bins	-1%	-2%	-15%	-29%
PC Ideal 140 kV 8 bins	-7%	-13%	-22%	-39%
PC Realistic 140 kV 2 bins	+58%	+149%	+39%	+95%
PC Realistic 140 kV 4 bins	+50%	+126%	+32%	+75%
PC Realistic 140 kV 8 bins	+42%	+101%	+24%	+54%
PC 90 kV / EI Sn 150 kV 1 bin	-5%	-10%	-13%	-24%
PC 90 kV / EI Sn 150 kV 2 bins	-9%	-17%	-17%	-30%
PC 90 kV / EI Sn 150 kV 4 bins	-10%	-19%	-17%	-32%
PC 90 kV / PC Sn 150 kV 1 bin	+10%	+21%	-2%	-4%
PC 90 kV / PC Sn 150 kV 2 bins	+2%	+5%	-10%	-19%
PC 90 kV / PC Sn 150 kV 4 bins	+1%	+3%	-11%	-21%



# Conclusion

- **Comparison of today's DECT approaches**
  - Dual source CT performs best, having the most flexibility
  - Fast kV switching performs a bit worse than DS DECT at 100 kV / Sn 140 kV
  - Sandwich detector's performance suffers from spectral overlap
- **Novel photon counting detector technology studied**
  - Very promising results and great patient dose saving possibilities in case of ideal detector: Up to 70% (iodine image) for 8 energy bins compared to DS DECT at 100 kV / Sn 140 kV
  - Undesired detector effects result in worse performance than today's gold standard (DS DECT at 100 kV / Sn 140 kV)
  - Dual source CT with photon counting detectors improves performance
    - Interesting future technology

# Thank You!



## The 4<sup>th</sup> International Conference on Image Formation in X-Ray Computed Tomography

July 18 – July 22, 2016, Bamberg, Germany  
[www.ct-meeting.org](http://www.ct-meeting.org)



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Conference Chair

Marc Kachelrieß, German Cancer Research Center (DKFZ), Heidelberg, Germany

This presentation will soon be available at [www.dkfz.de/ct](http://www.dkfz.de/ct).

This work was supported by the Deutsche Forschungsgemeinschaft (DFG) under grant KA 1678/5-1 and LE 2763/1, and by the German Government, Bundesministerium für Bildung und Forschung (01EX1012B, Spitzencluster Medical Valley).

The reconstruction software was provided by RayConStruct<sup>®</sup> GmbH, Nürnberg, Germany.